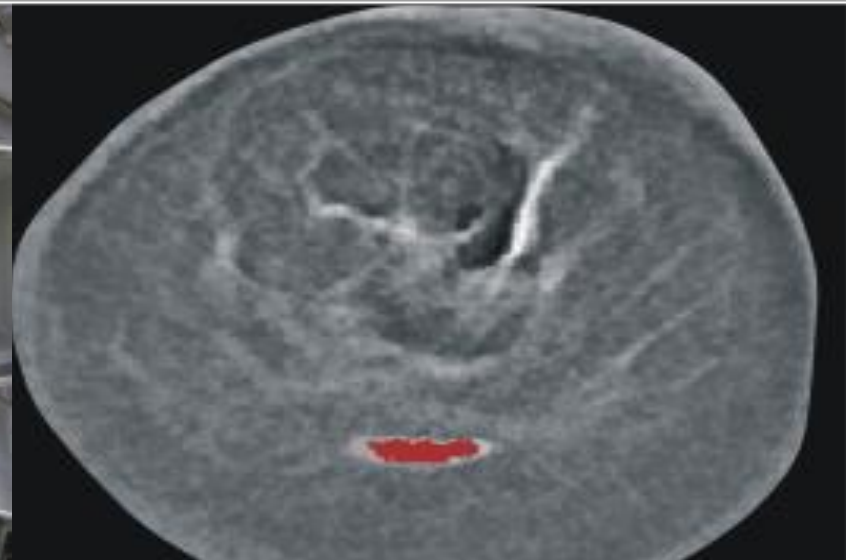


3D Image Reconstruction: Ultrasound Tomography for Breast Cancer Diagnosis

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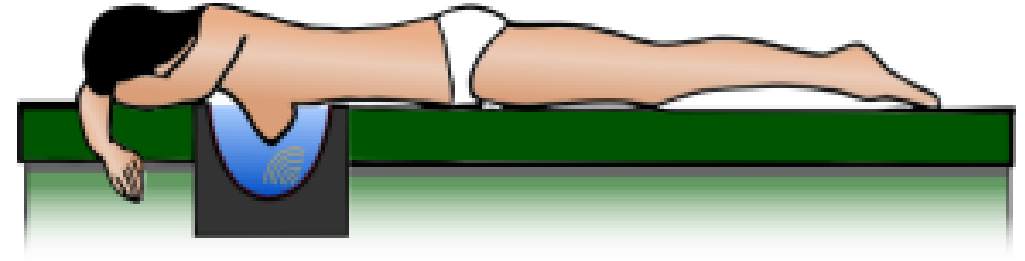
3D USCT and Breast Cancer

Basic idea

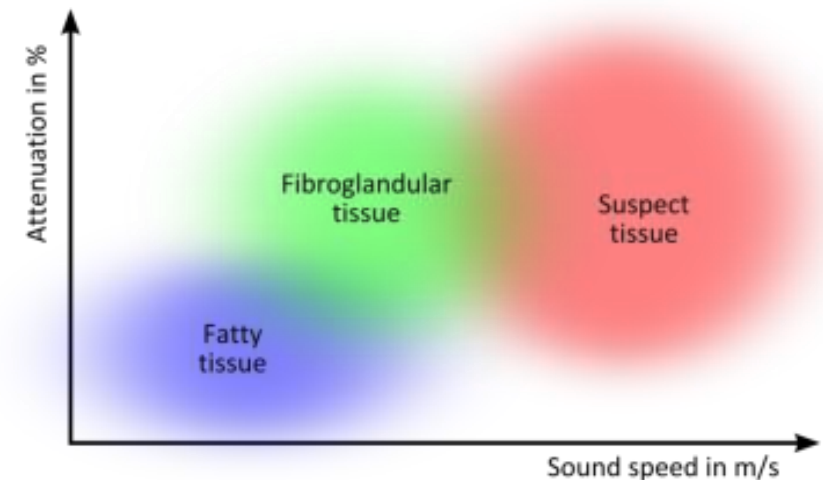
- Surround object with (unfocused) ultrasound transducers in a fixed setup

Diagnostic value

- Reproducible 3D images with ultrasound
- Images three modalities concurrently:
 - **Reflection**
High quality “B-scans”
 - **Speed of sound and attenuation**
Quantitative information

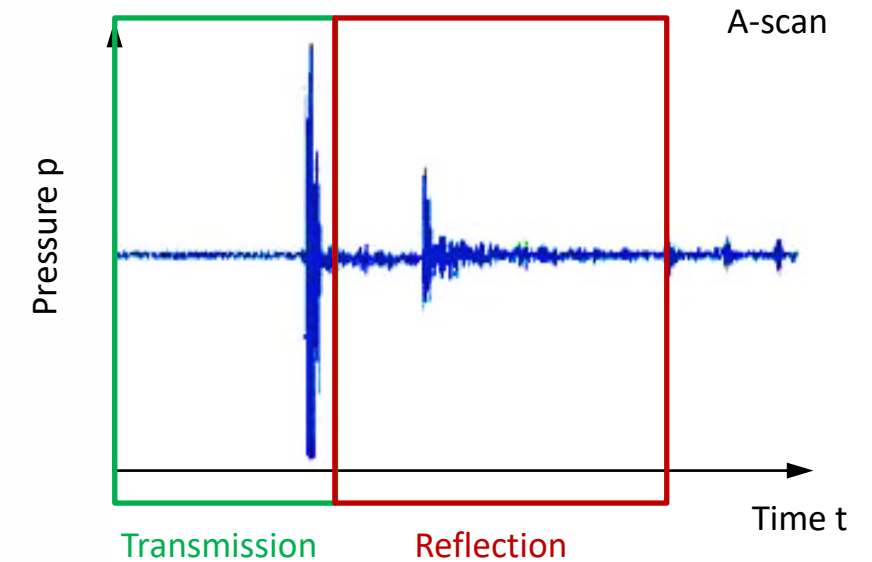
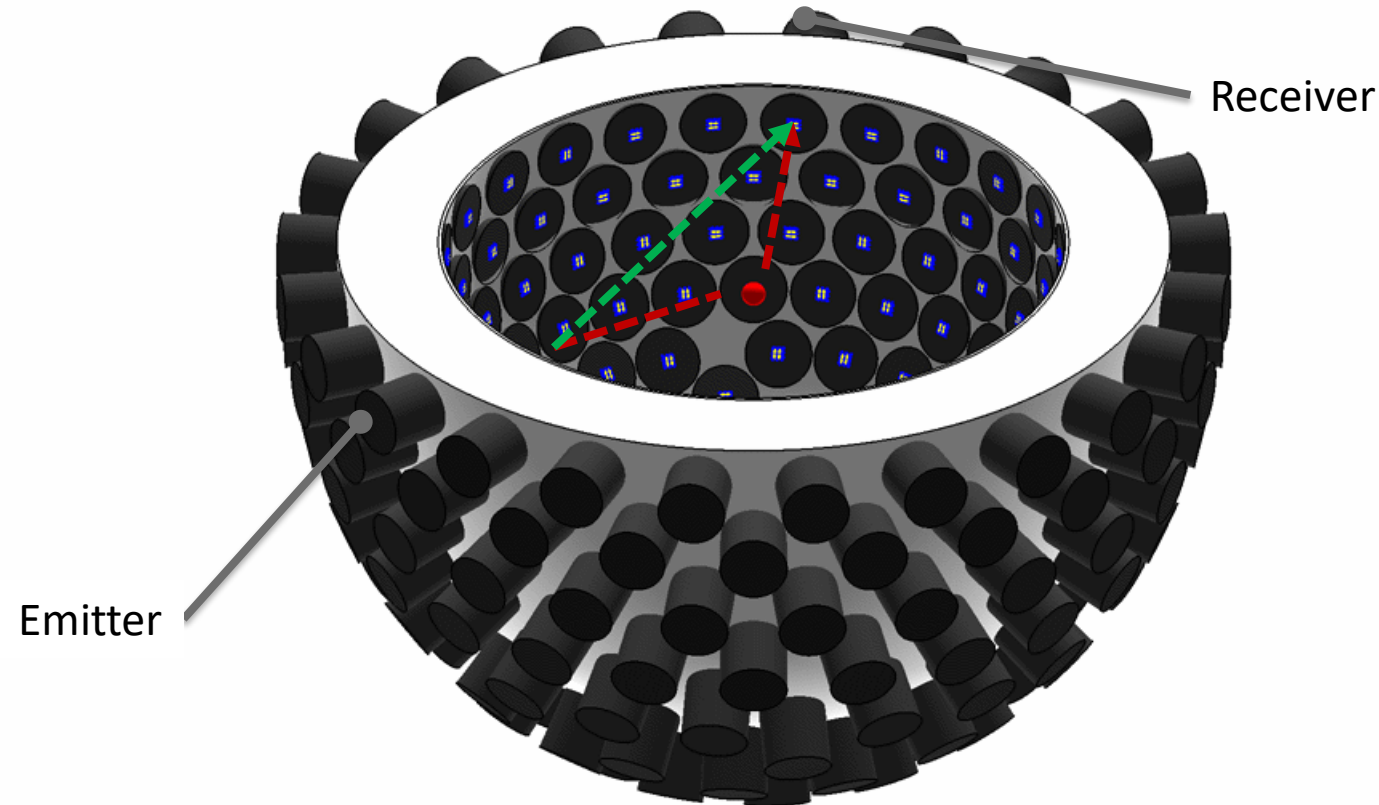


Breast imaging in fixed setup



Simplified from Greenleaf et al., 1981

How does it work? Data acquisition



- Thousands of transducers
- High data rates
- Small signals



Acquired information

- Sound speed
- Attenuation
- Reflection

KIT 3D USCT II and USCT III



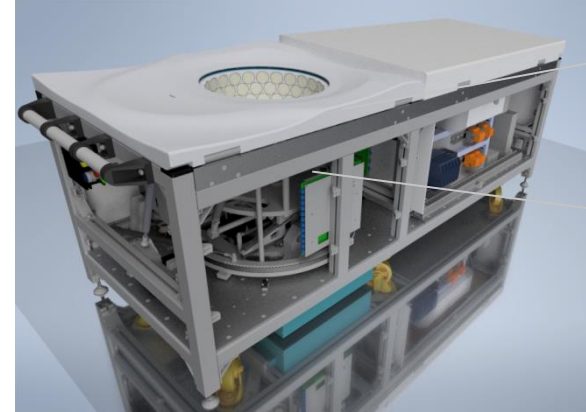
KIT 3D USCT II



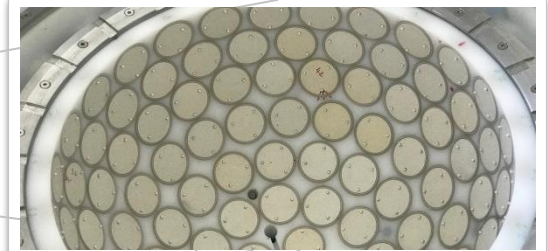
Measurement aperture



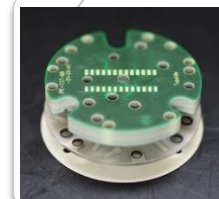
Transducer Array System



KIT 3D USCT III



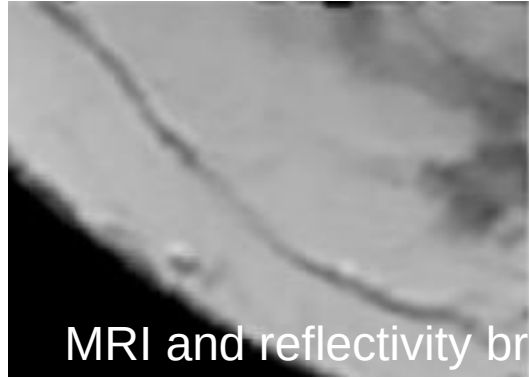
Measurement aperture



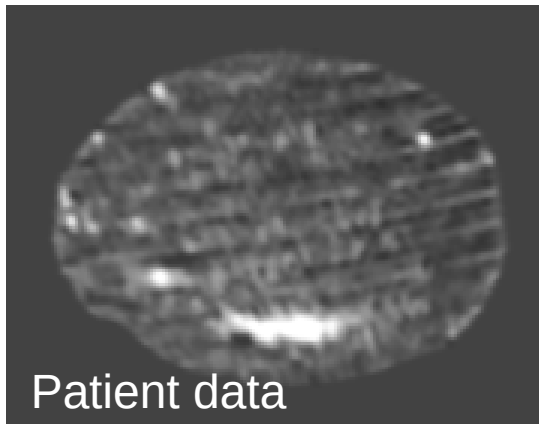
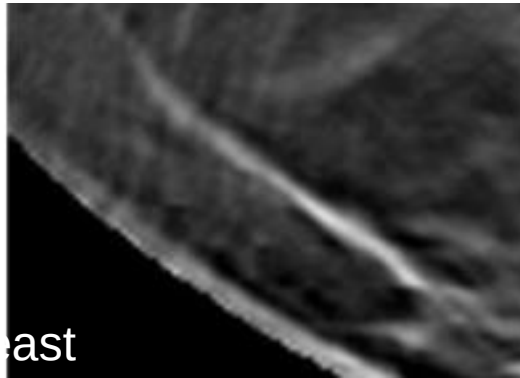
Transducer Array System

Specification	Value
Center frequency (bandwidth)	2.5 MHz (50%-70%)
Highest resolution	$(\lambda/2)^3 \approx (0.24 \text{ mm})^3$
# transducers	2041 - 2304 (sparse!)
Diameter (in meter and wavelength)	0.24 -0.32 m ($\sim 500 \lambda$)

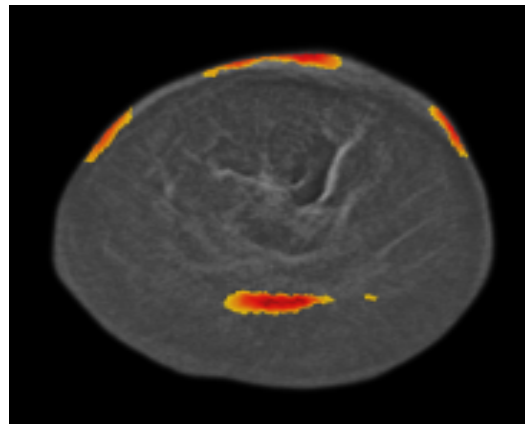
Some results



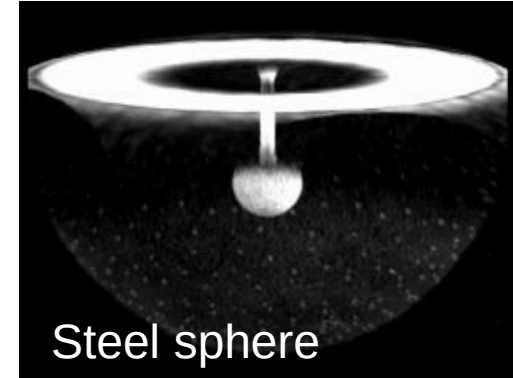
MRI and reflectivity breast



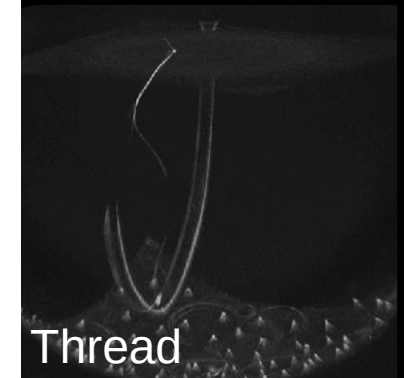
Patient data



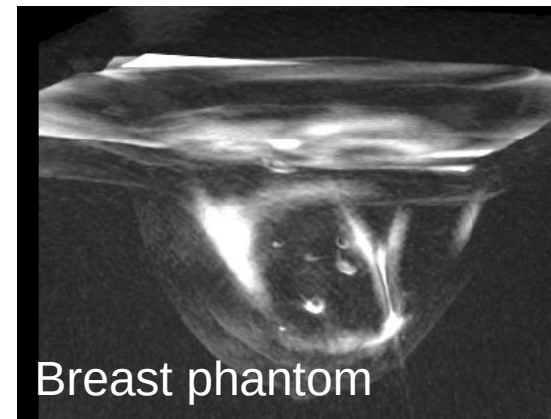
3D USCT II



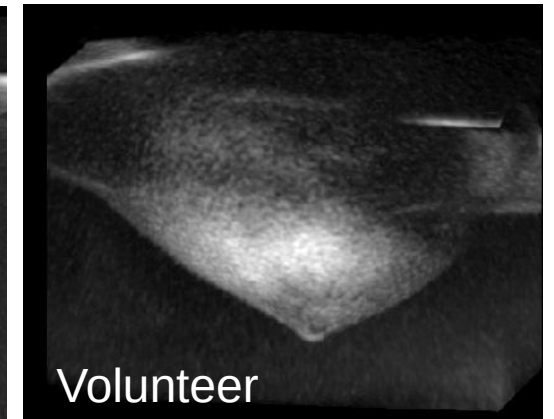
Steel sphere



Thread



Breast phantom



Volunteer

3D USCT III

Image Reconstruction: Acoustic Wave Equation

- Linear acoustic wave equation for inhomogeneous water like materials:

$$\nabla^2 p(\vec{x}) + k_0^2 \left(\sqrt{\frac{K_0}{\rho_0}} \sqrt{\frac{\rho(\vec{x})}{K(\vec{x})}} + i \frac{\mu(\vec{x})}{k_0} \right)^2 p(\vec{x}) - \frac{1}{\rho(\vec{x})} \nabla \rho(\vec{x}) \nabla p(\vec{x}) = 0$$

- Three physical properties influence wave propagation:

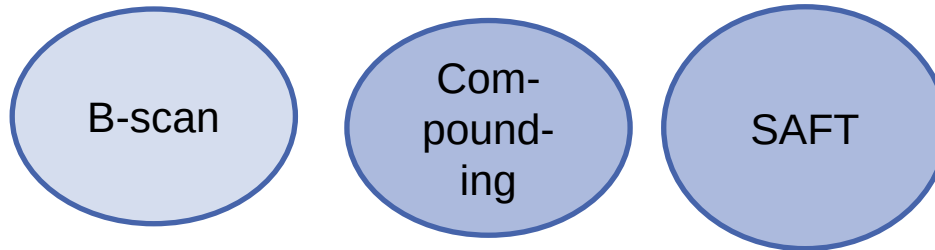
- Density ρ_0
- Bulk modulus K
- Absorption μ

- Typically reconstructed in USCT:

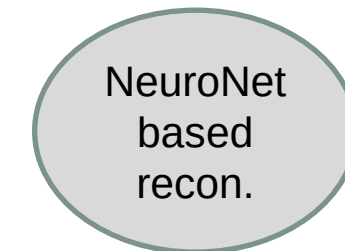
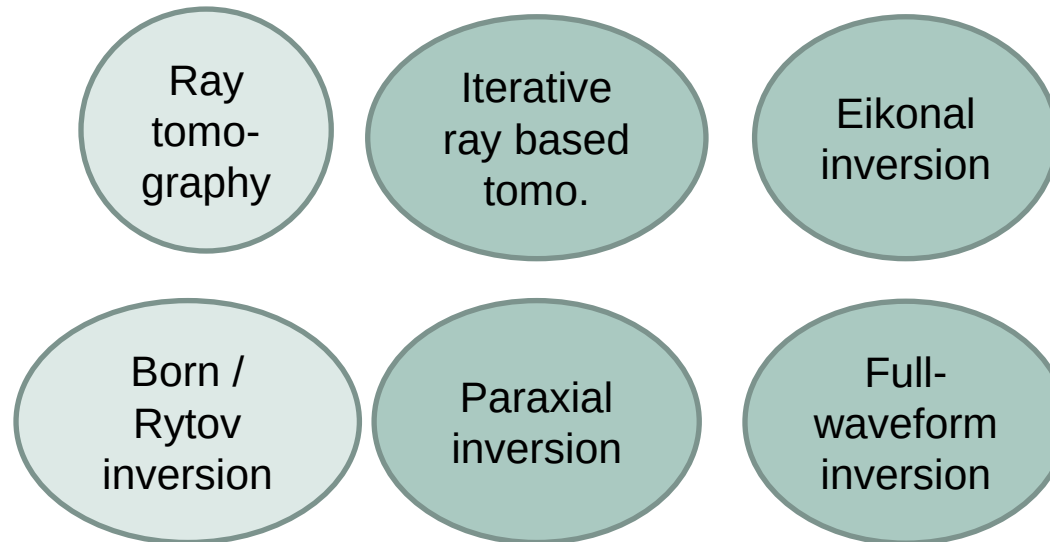
- Qualitative gradient of acoustical impedance $\nabla(Z = \rho_0 c)$,
- Speed of sound $c = \sqrt{\frac{K}{\rho_0}}$,
- Attenuation $\alpha = \mu + \mu_s$

Image reconstruction: Typically used methods

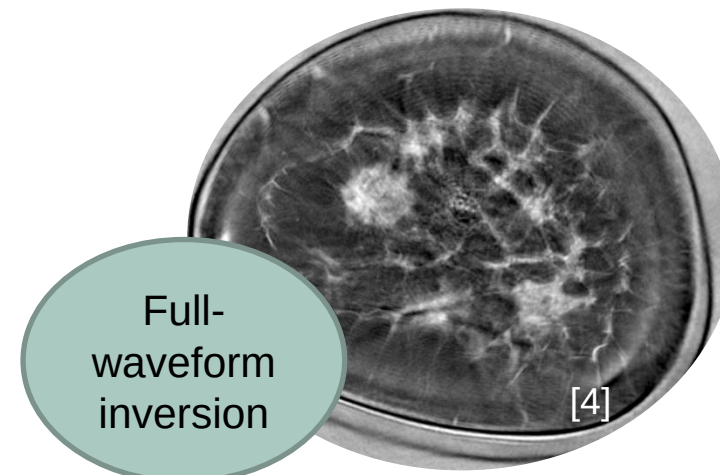
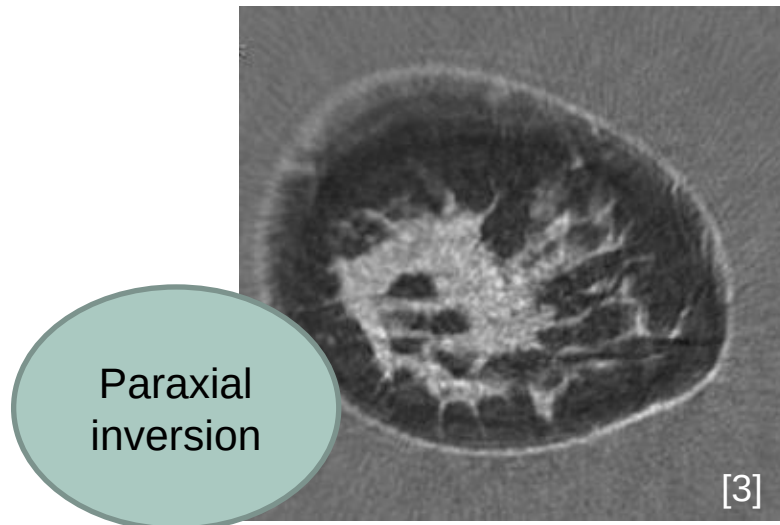
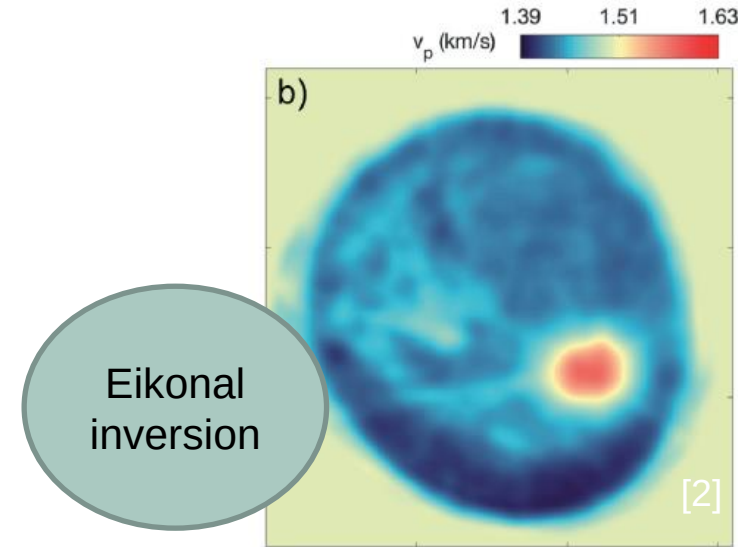
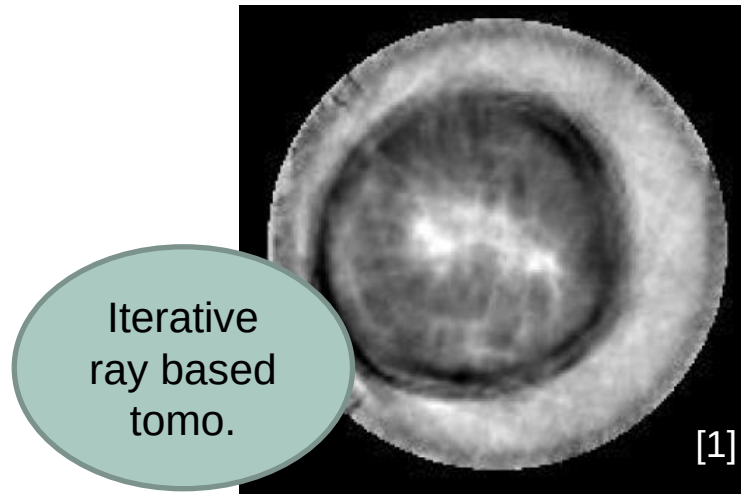
■ Reflectivity (Qualitative gradient of acoustical impedance):



■ Speed of sound and attenuation

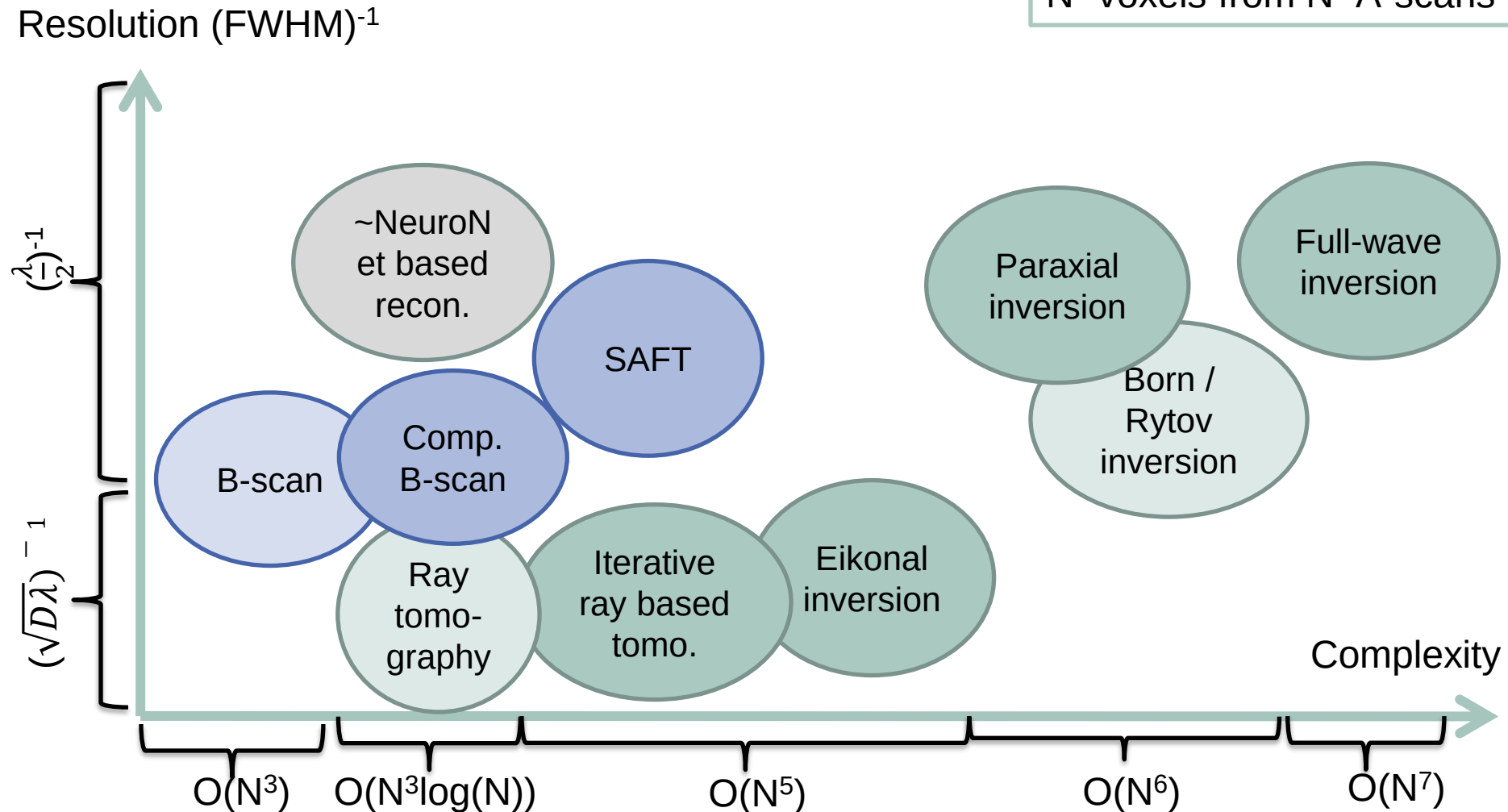


Breast Image Examples: 2D Speed of Sound



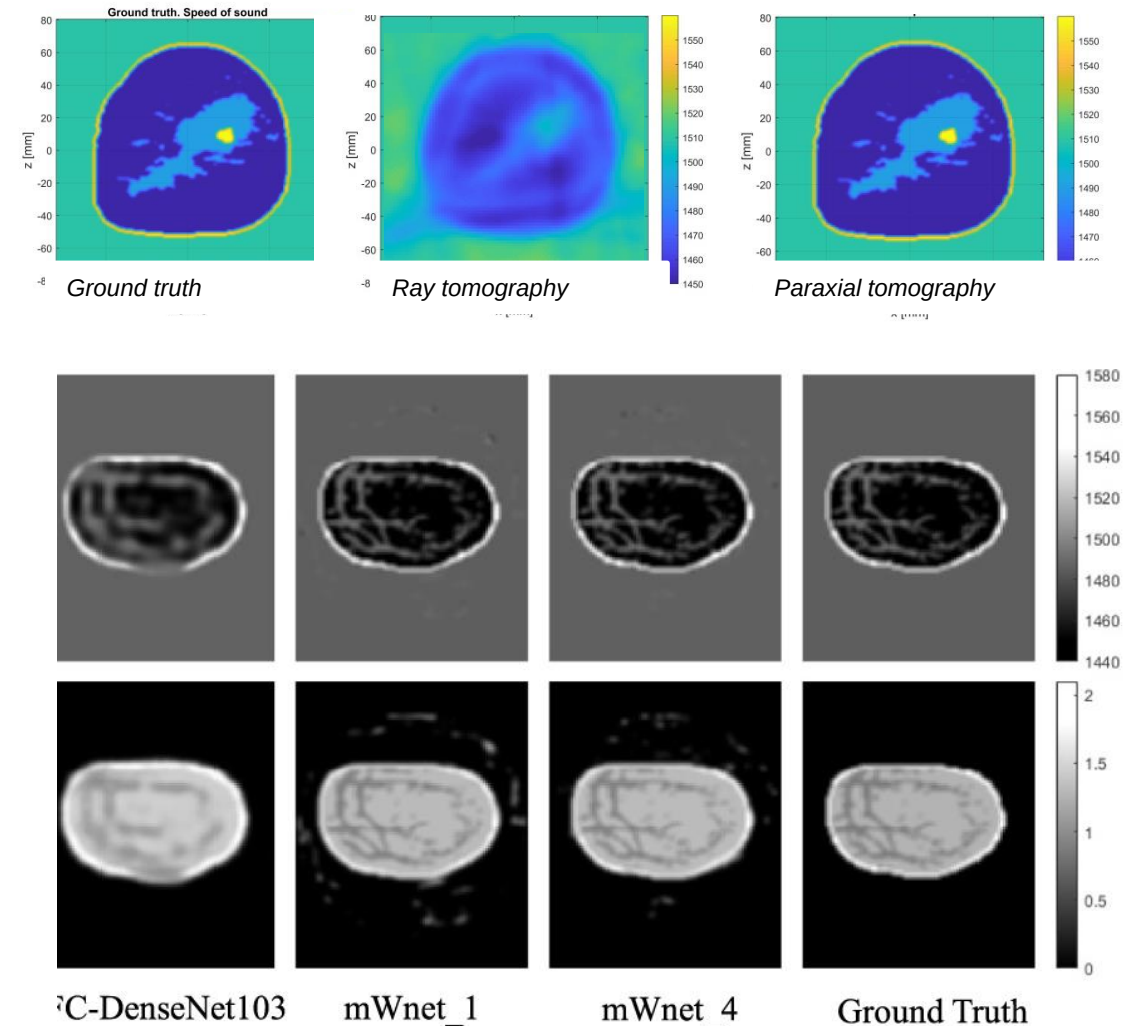
Challenge 3D: Computational Complexity

Example:
 N^3 voxels from N^2 A-scans



Status at IPE

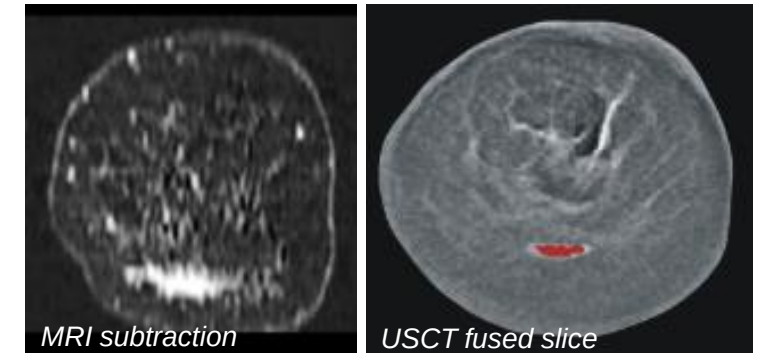
- Applied algorithms in clinical trials:
 - Speed of sound corrected SAFT with GPU cluster
 - Ray based speed of sound and attenuation
- Under development
 - Paraxial
 - Neuronal networks based reconstruction
- New grant (EIC pathfinder):
 - 3D FWI on supercomputers



Reconstruction with Prelearned Convolutional Neural Network (simulated data)

Summary and possible collaborations

- 3D USCT is a new imaging method for early breast cancer diagnosis
- KIT 3D USCTs:
first clinically applicable full 3D USCT
- New improved system in commissioning
- First pilot study successful,
multicenter study planned



Possible collaboration

- Challenge: 3D, large scale problem, limited reconstruction time!
- Efficient solution of large scale inverse problem?
 - Optimization schemes, ...
- Efficient forward method
 - Approximation(s) of wave equation for dedicated problem, ...
- Neuronal networks
 - Learning parts of the image reconstruction problem?
 - Direct learning from data input to image output?
- Perspective topics: algorithms dedicated for future computing architectures
 - E.g. applicable problem for quantum computing?

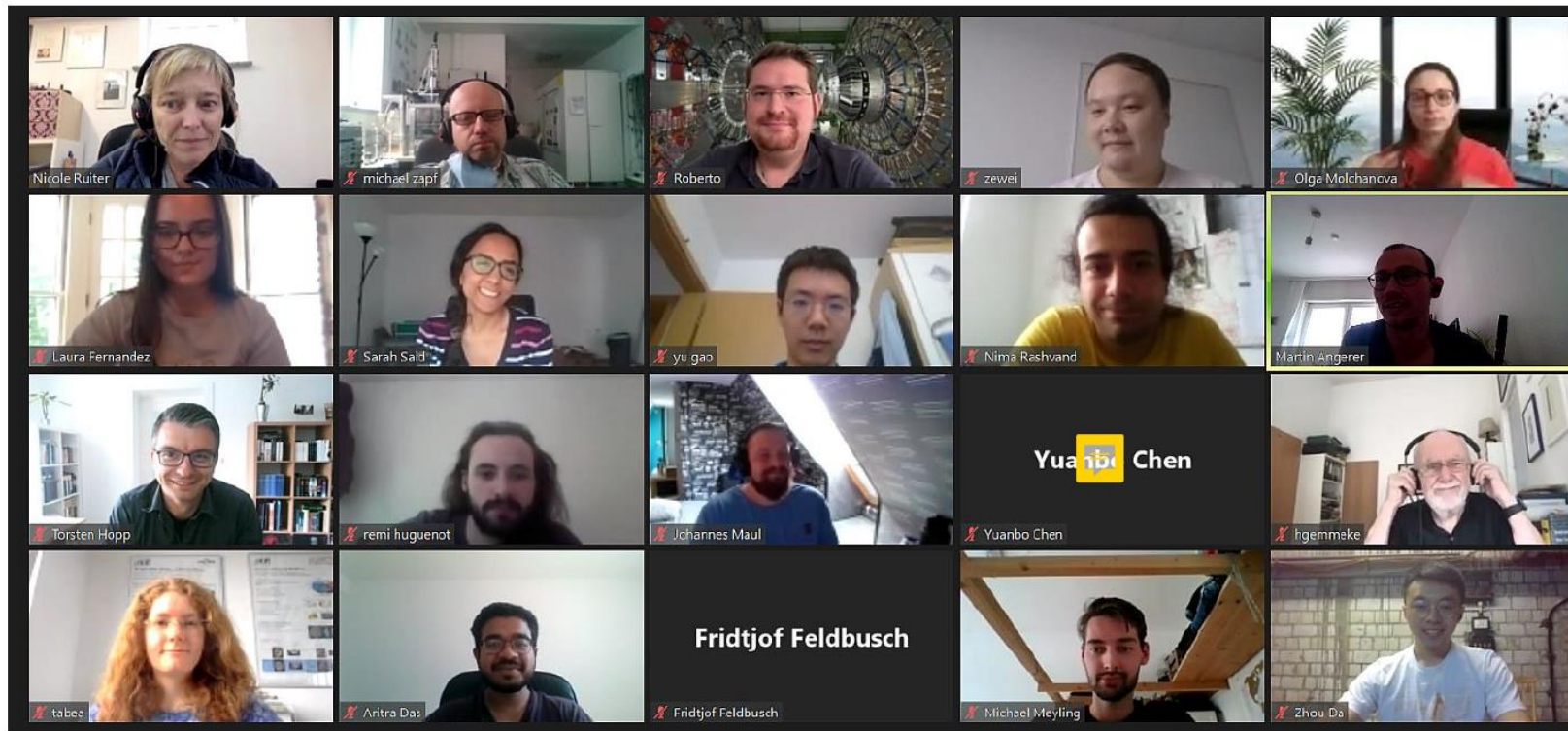
Thank you!



Imperial College
London



FrontWave Imaging



European
Innovation
Council



DFG
HEIKA

