

PHILIPS

sense and simplicity

Digital Photon Counters as Scalable Building Blocks for Various Applications

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Heraeus Seminar Bad Honnef
May 23rd, 2013

What is Philips Digital Photon Counting (PDPC) doing ?

Philips Digital Photon Counting is designing and manufacturing **scalable** detectors based on **digital Silicon Photomultiplier (dSiPM) technology** – a new type of advanced solid state light detector, now called **Digital Photon Counter (DPC)**.

Potential Applications

- Medical Imaging
- Life Sciences
- High Energy Physics
- Material Testing/Detection
- Process Control



Solid State, Digitization & Integration Win

Transistor



Television



Photography



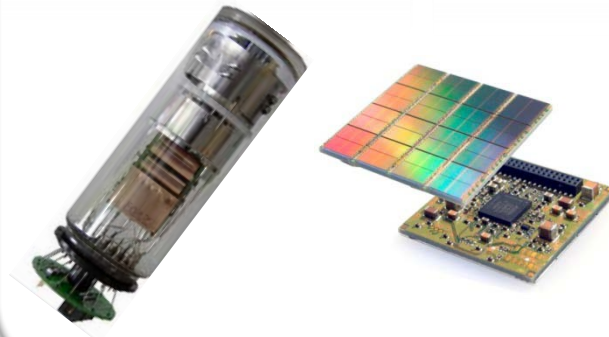
Telephony



X-Ray imaging



Next: Light Detection



Disruptive Technology: Example TV/displays



- **size/format:**

- just standing on support
- big 3D box
- size limited by tubes

- wall hanging
- almost 2D, displays everywhere
- flat, no size limitation

- **image quality:**

- 60/100/200 Hz flickering
- initially higher resolution
- limited contrast

- no flickering anymore
- resolution nearly unlimited
- real life contrast

- **functionality:**

- just TV or PC display
- single medial

- internet, TV and PC merge
- multi-medial

- **safety:**

- HV
- vacuum, risk of implosion

- no HV
- no risk of implosion

Outline

Concept of scalability, from pixels to systems

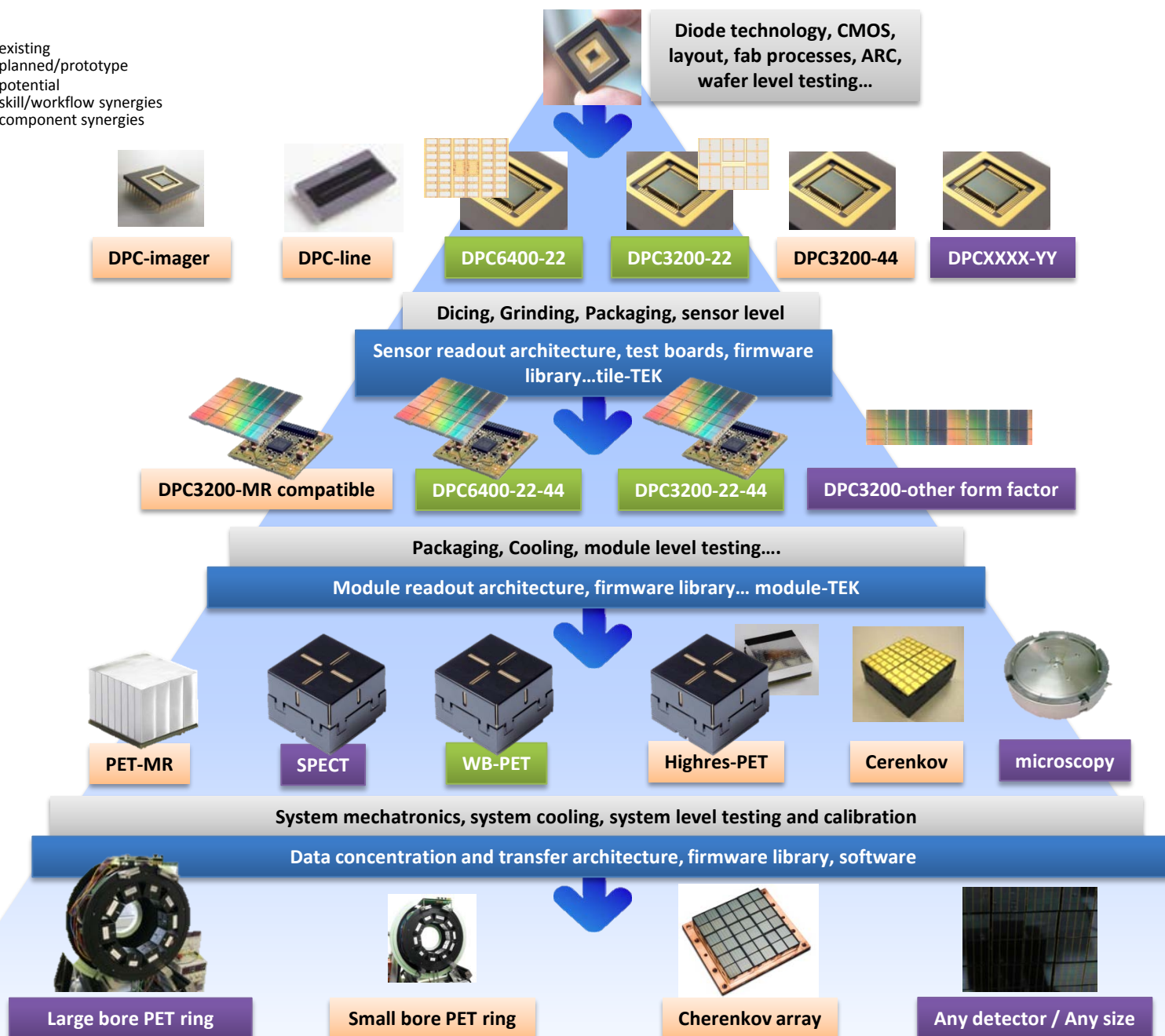
Applications

- Positron Emission Tomography
- Cerenkov light detection

Outlook

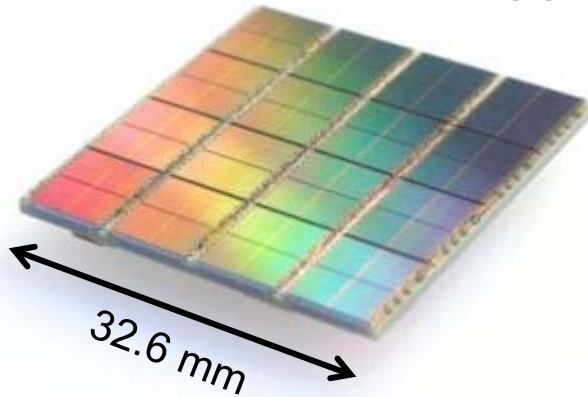
The Philips tree of scalable DPC technology

- existing
- planned/prototype
- potential
- skill/workflow synergies
- component synergies



Digital Photon Counters enable Integrated “Intelligent” Sensors

DPC3200-22-44

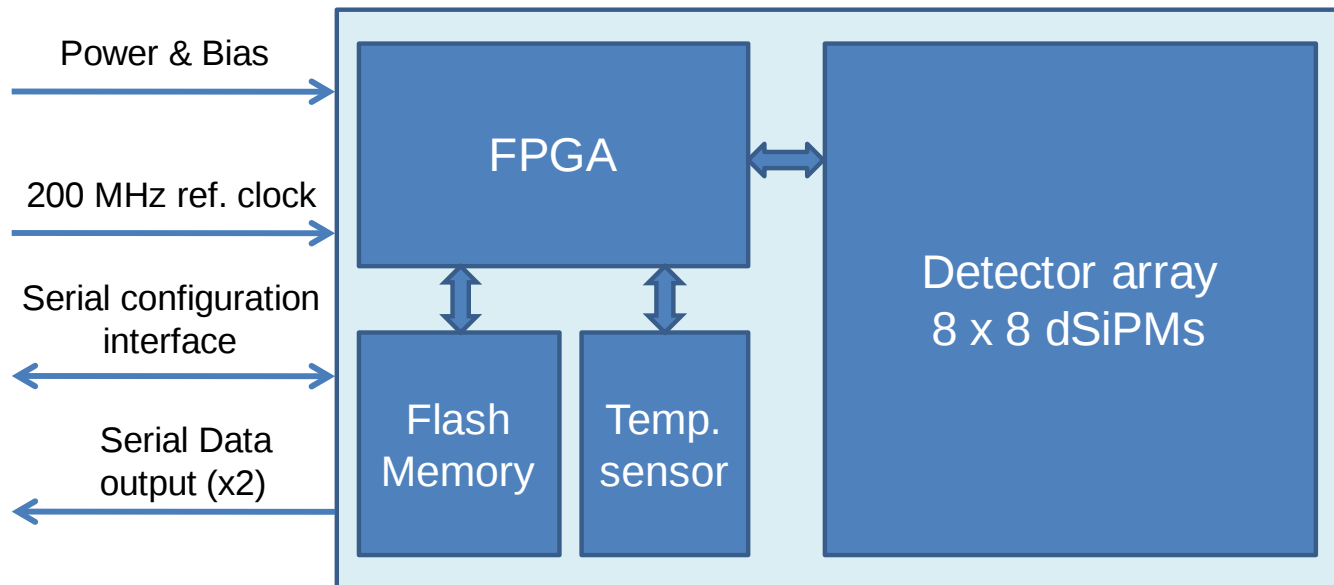


FPGA

- Clock distribution
- Data collection/concentration
- TDC linearization
- Saturation correction
- Skew correction

Flash

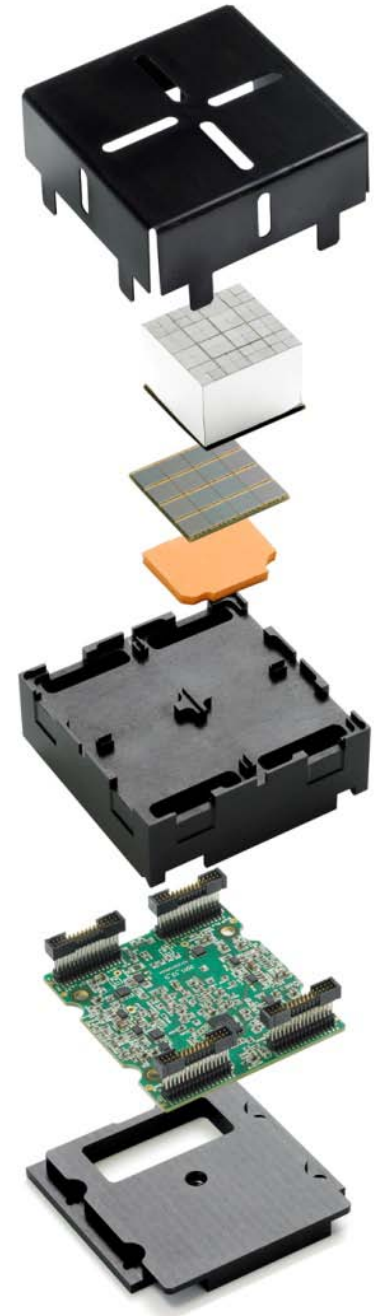
- FPGA firmware
- Configuration
- Inhibit memory maps



Further integration: Detector Module



- Modular design incl. 2 x 2 tiles, approx. 6.6 x 6.6 cm²
- Module PCB for power supplies, data concentration, processing & corrections
- Designed for easy cooling

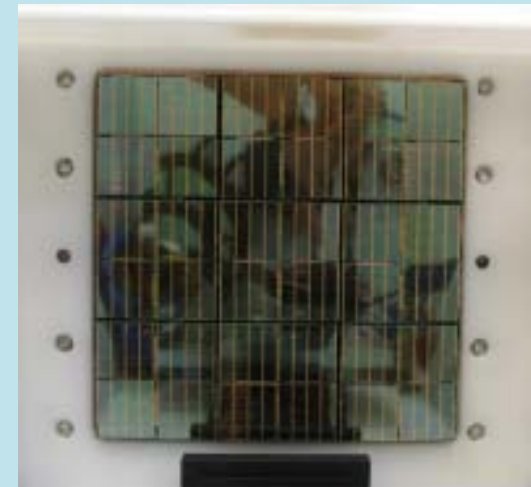
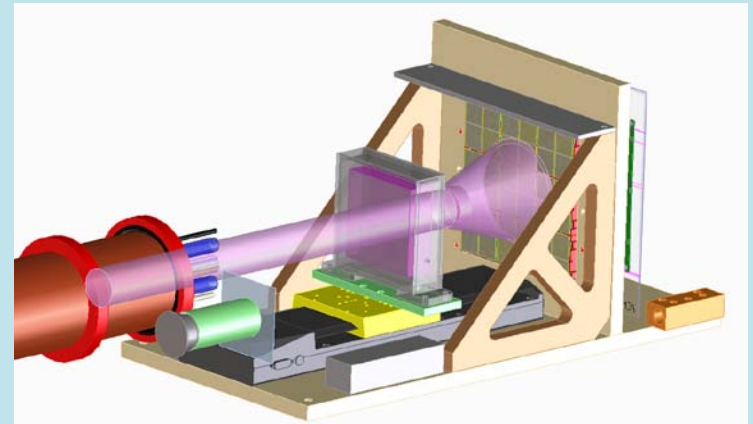


Integration into Systems

Medical Imaging: Positron Emission Tomography



High Energy Physics: Cerenkov detector



Application Example

Positron Emission Tomography (PET)

Positronen-Emission-Tomography (PET) as an application for DPCs



Positron-Emission-Tomography (PET)

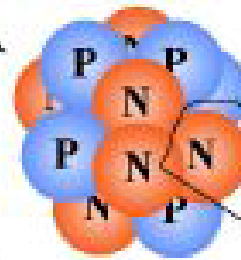
1.) **Production of isotopes** with proton excess in compact cyclotrons (e.g. ^{11}C , ^{13}N , ^{15}O , ^{18}F)



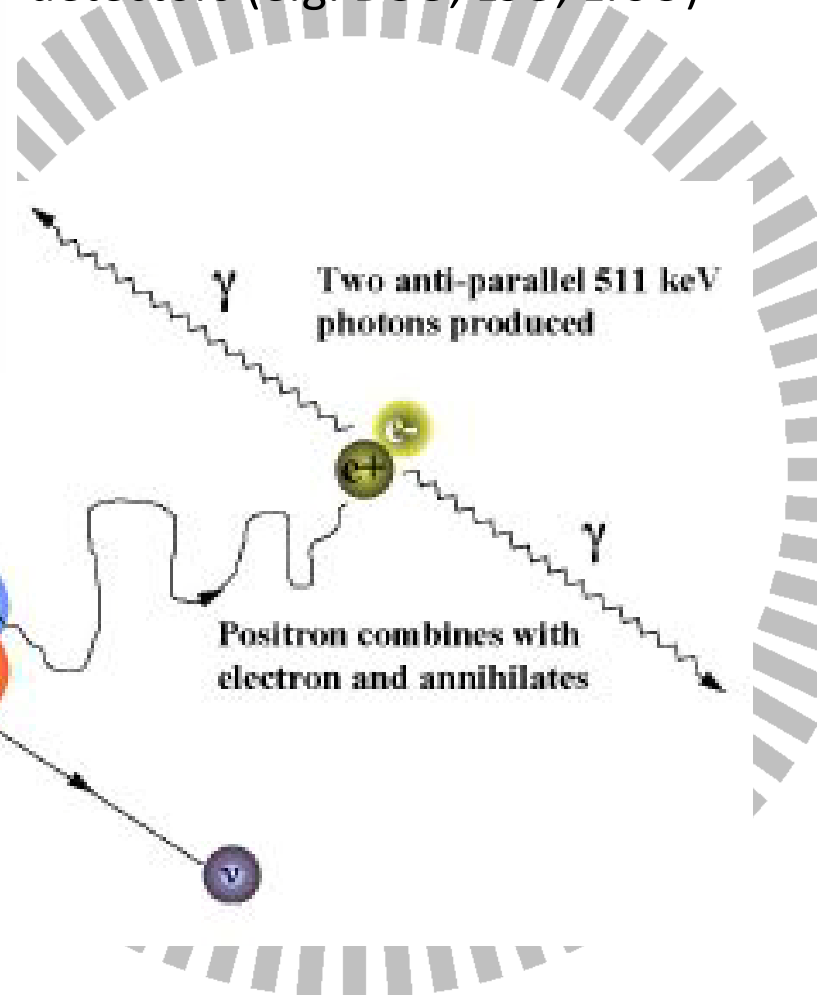
2.) **Labeling of organic molecules** with positron emitting isotope (e.g. ^{18}F FDG) - **tracer**



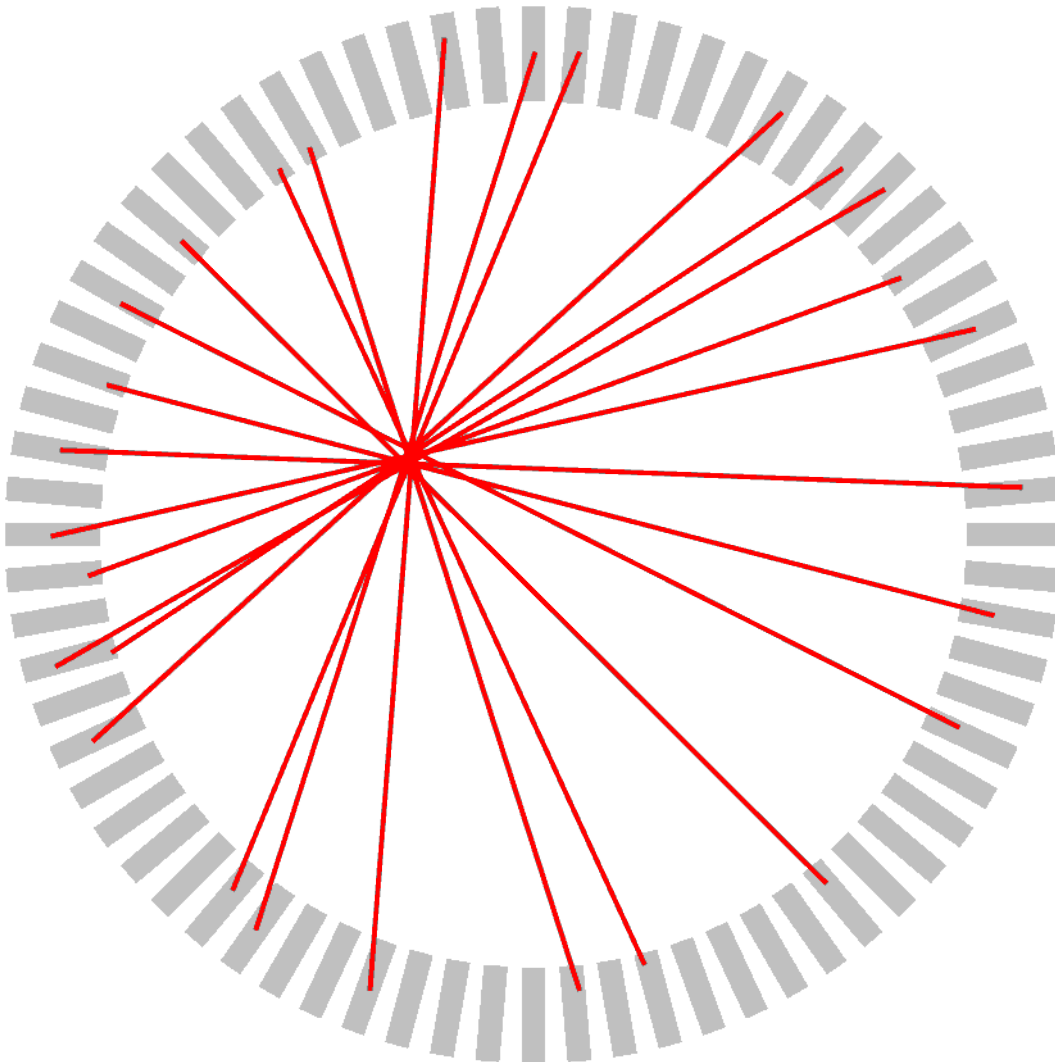
Proton decays to neutron in nucleus - positron and neutrino emitted



3.) **Detection of 511 keV** annihilation γ -radiation with ring of scintillation detectors (e.g. BGO, LSO, LYSO)



PET – The Principle



Inject tracer

Wait (~60 min)

Marker accumulates

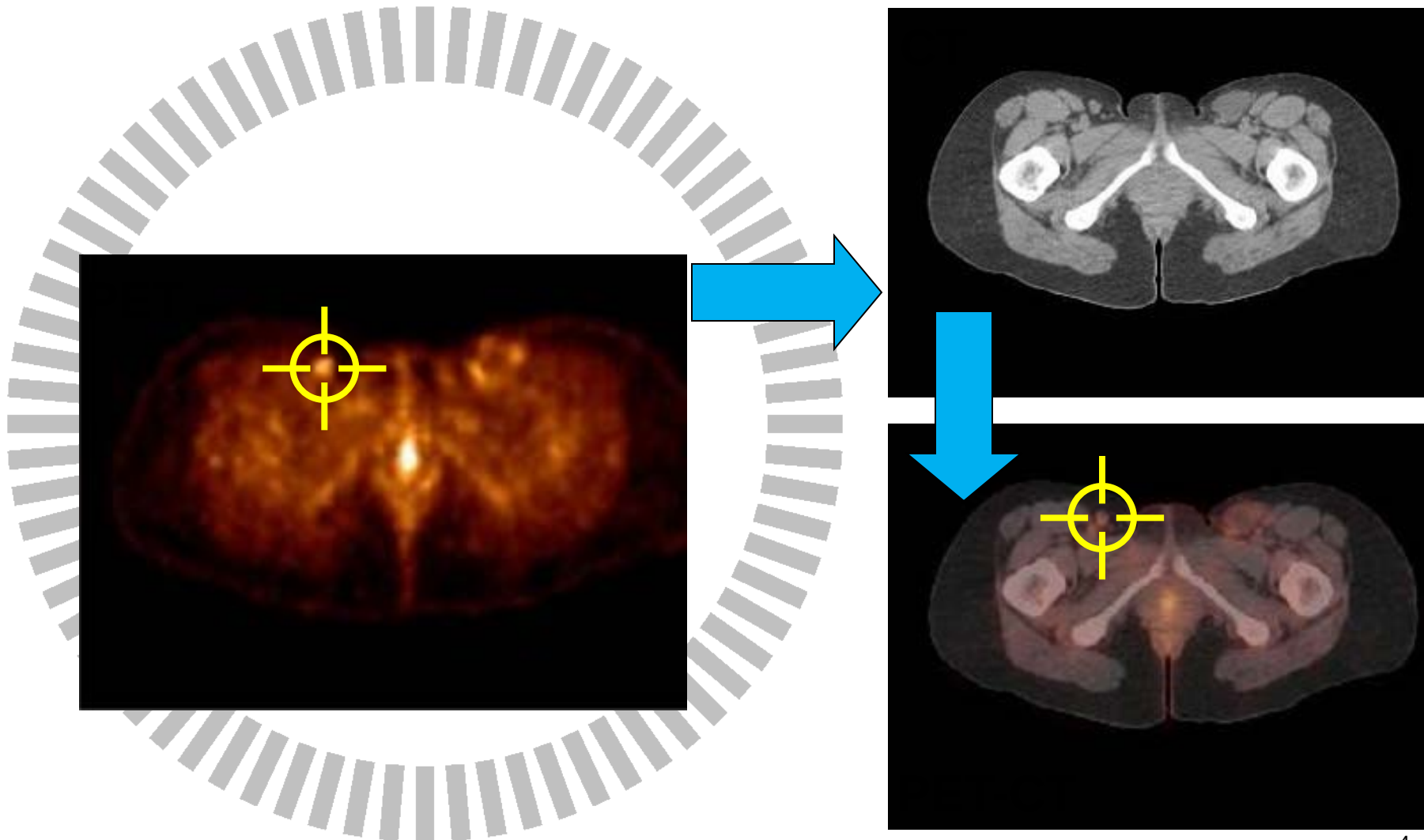
β^+ annihilation emits
two γ under 180°

Detect coincident γ
with ring detector

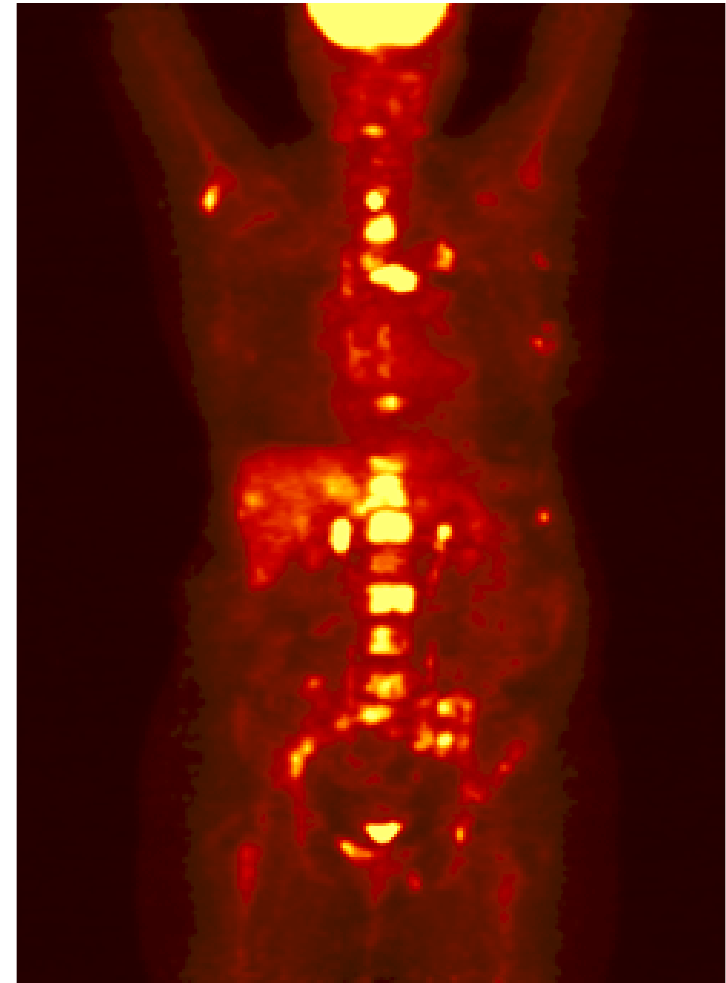
Acquire $\sim 10^8$ LORs
(lines-of-response)

Reconstruct 3D
tracer distribution

PET – The Principle



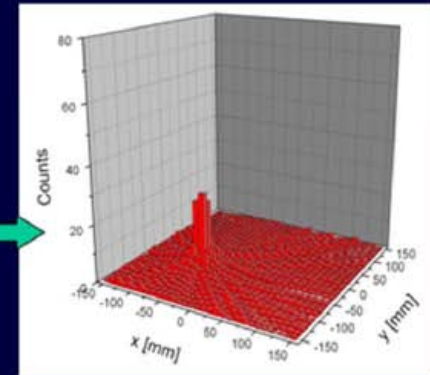
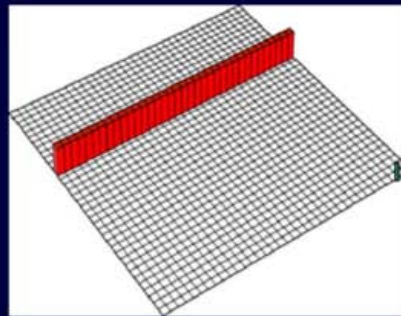
PET – The Principle



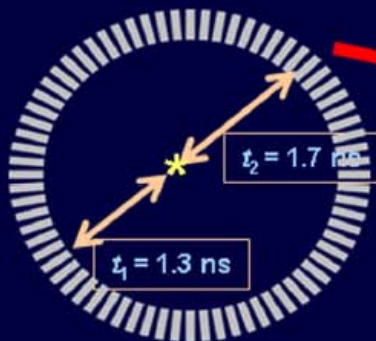
Time-of-flight (TOF-) PET

Time of Flight PET Systems

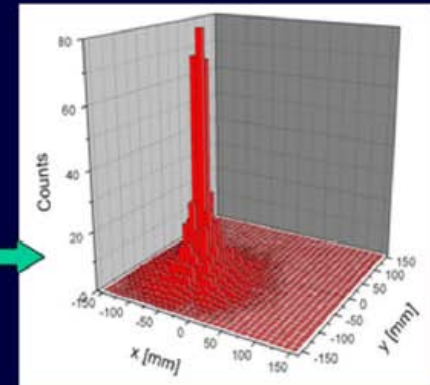
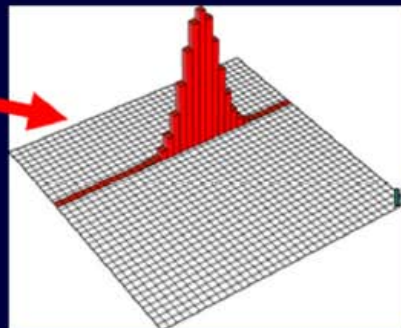
Conventional PET/
ToF off



Time-of-Flight PET



$t_2 - t_1$

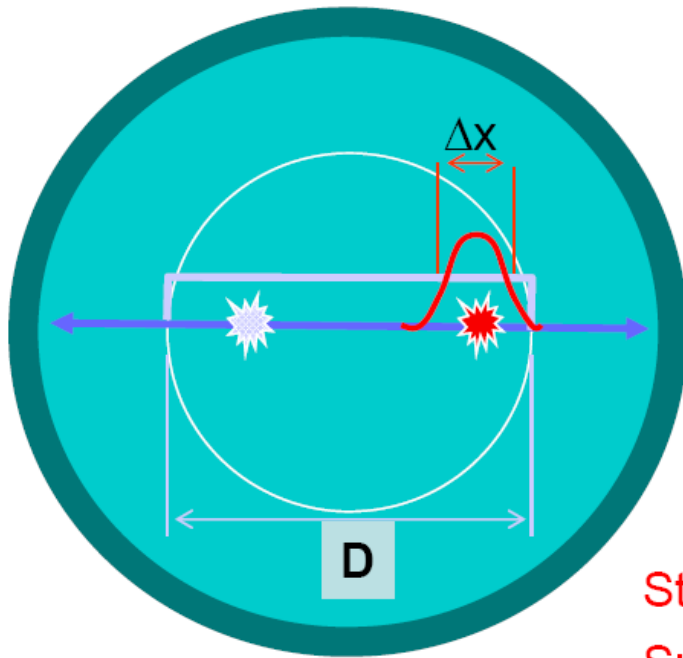


→ ToF: more signal, less noise

(TOF-) PET effect increases with reduced CRT and for larger objects

The accuracy of source position localization along line of response depends on the *coincidence resolving time (CRT)*

Δx = uncertainty in position along LOR = $c \cdot CRT/2$,
where c is the speed of light.



The TOF benefit is proportional to $D/\Delta x$,
where D is the effective patient diameter.

=> The smaller the CRT, the better.

State-of-the-art: $CRT \approx 500 \text{ ps} \Rightarrow \Delta x \approx 7.5 \text{ cm}$

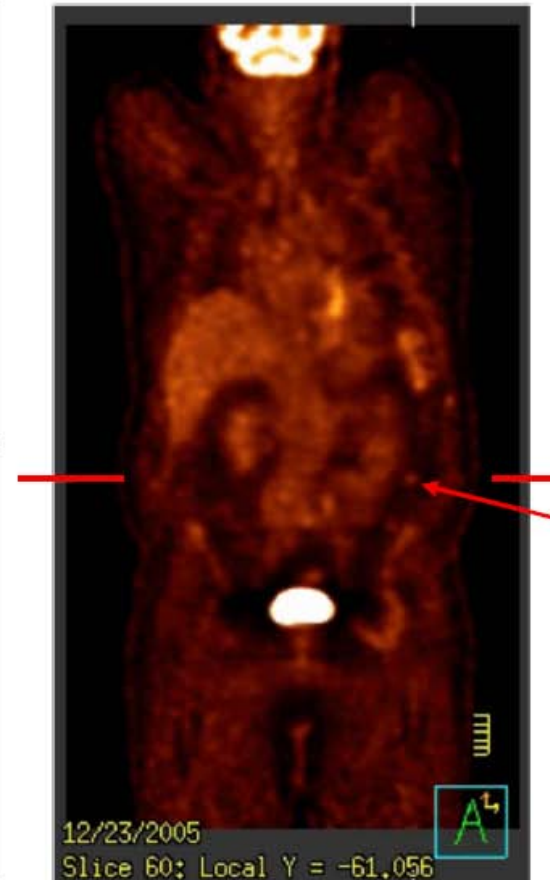
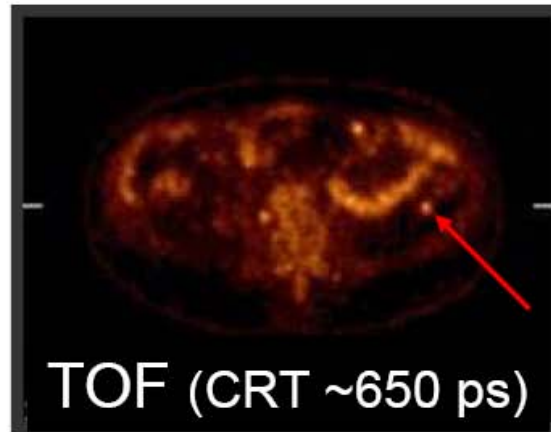
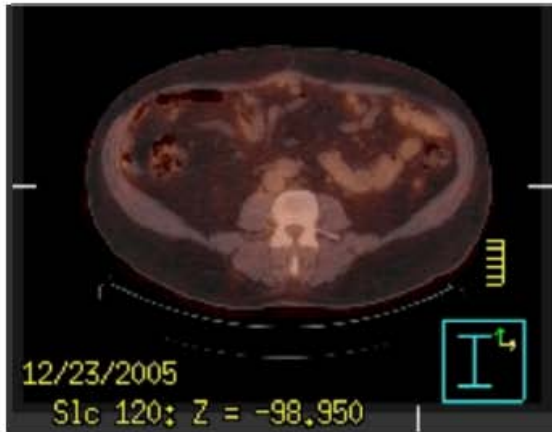
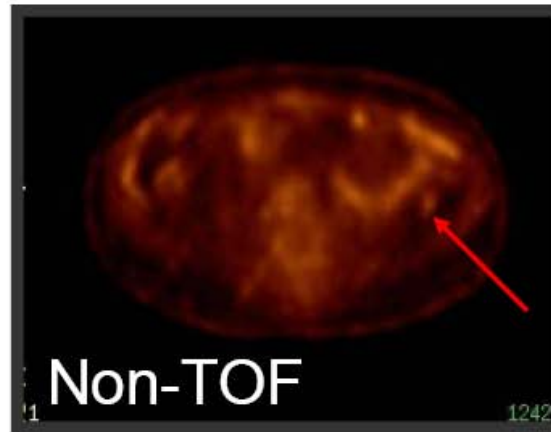
Suppose $CRT = 100 \text{ ps} \Rightarrow \Delta x = 1.5 \text{ cm}$

Graph courtesy of D. Schaart, Technical University of Delft, The Netherlands

Time-of-flight (TOF-) PET: IQ improvement

Colon cancer, left upper quadrant peritoneal node

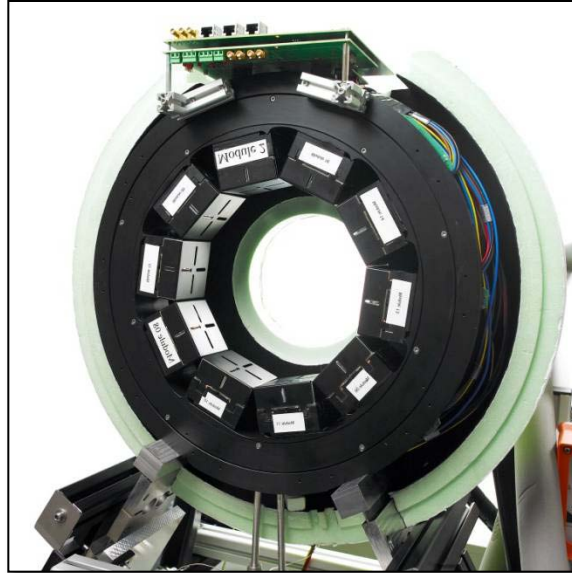
114 kg; BMI = 32.2
13.4 mCi; 2 hr post-inj



State-of-the-art clinical PET: coincidence resolving time (CRT) $\approx$ 500 ps

Images courtesy of J. Karp, University of Pennsylvania, Philadelphia

Prototype PET Scanner



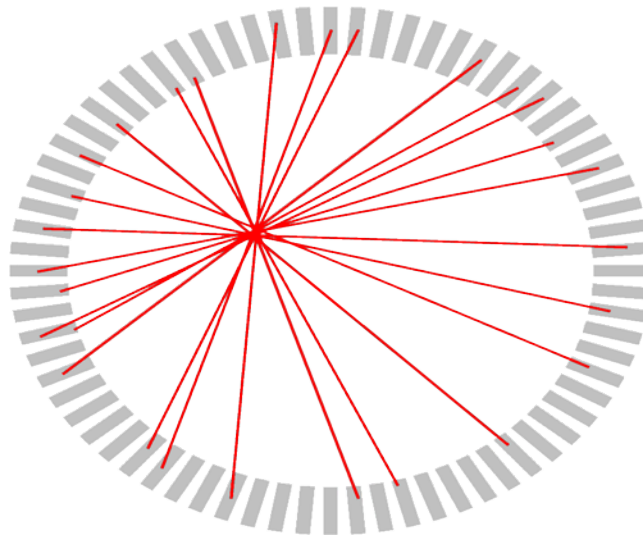
- 10 modules
- 20 cm transverse field-of-view
- 6.6 cm axial field-of-view
- 4x4x22 mm³ LYSO crystals, 1:1 coupling to DPC pixels
(not intended to be a high resolution scanner)
- Integrated cooling (5 – 10 °C operating temperature)



The challenge: information density



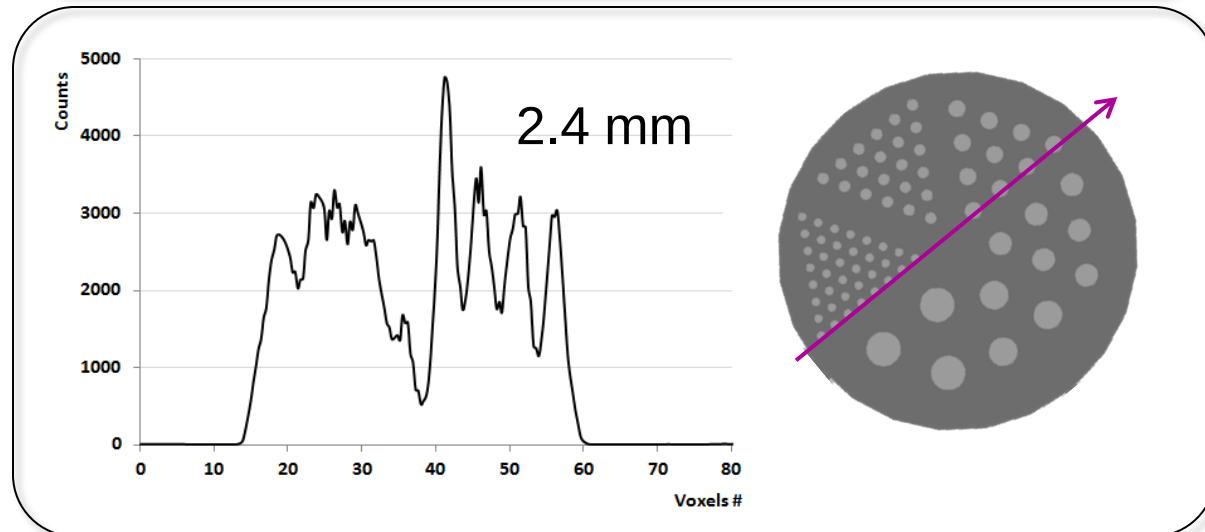
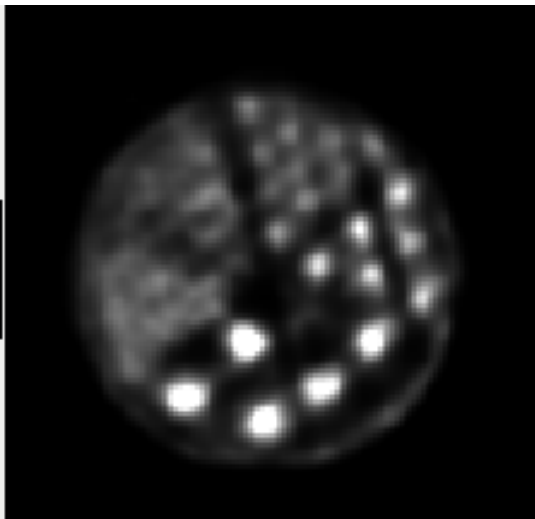
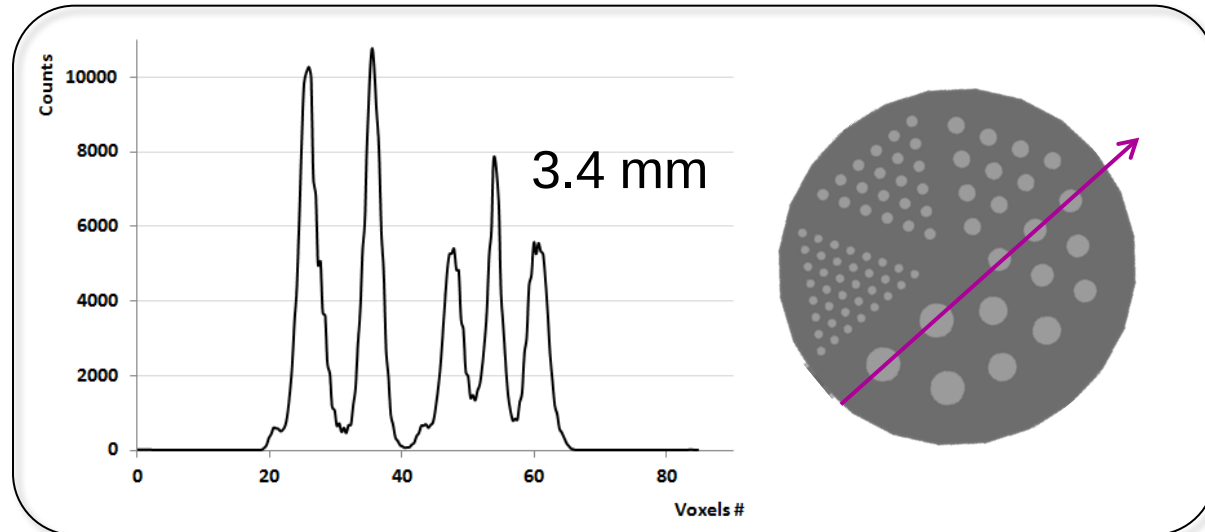
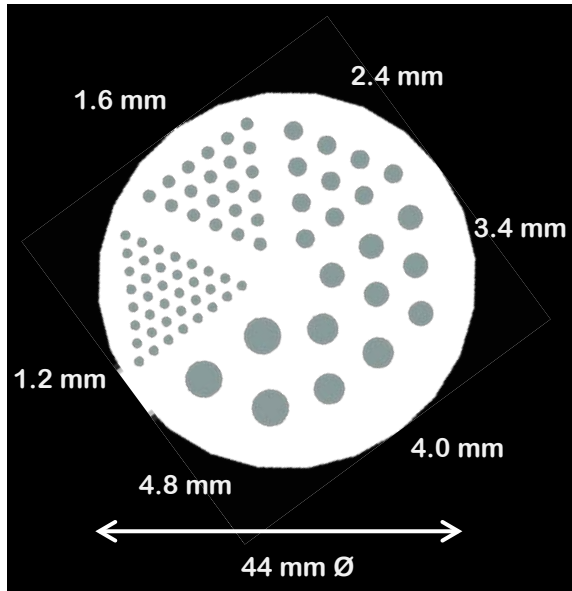
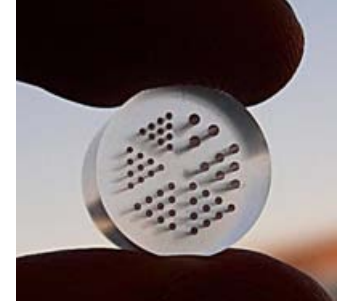
PMT-PET:
 $O(100)$ channels



Solid state PET:
 $O(10^4 - 10^5)$ channels

Spatial Resolution of Prototype Ring

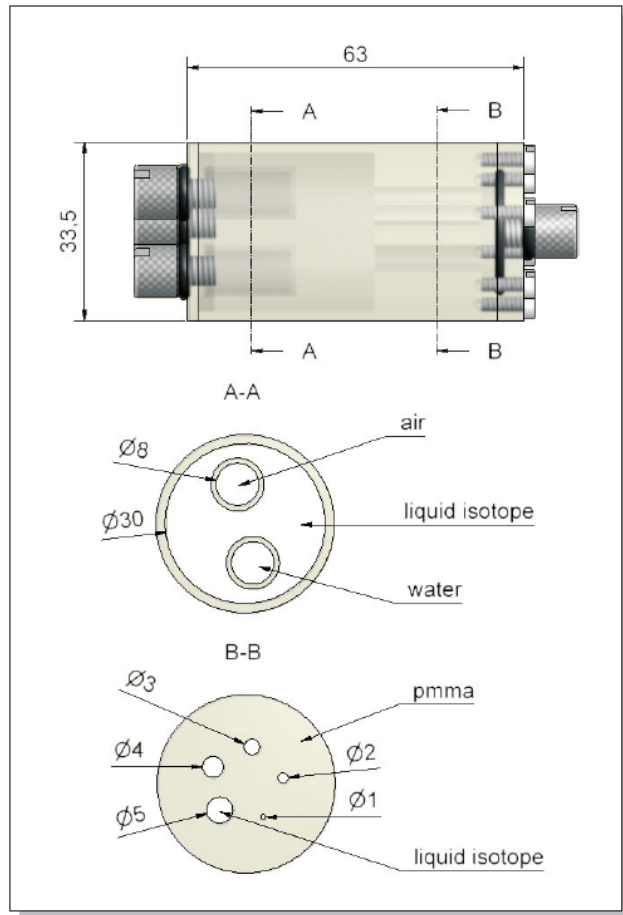
Mini Deluxe Derenzo Phantom



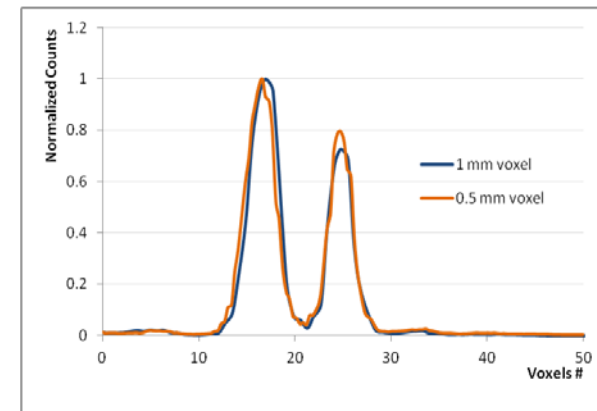
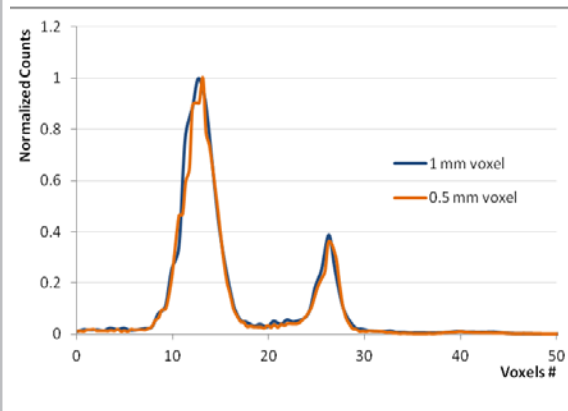
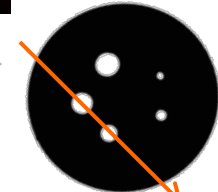
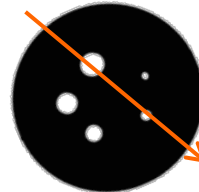
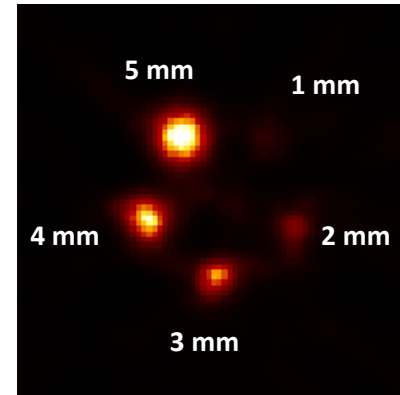
Spatial Resolution of Prototype Ring

NEMA NU-4 quality phantom

*Micro-PET IQ Phantom
(according to NEMA NU 4-2008)*



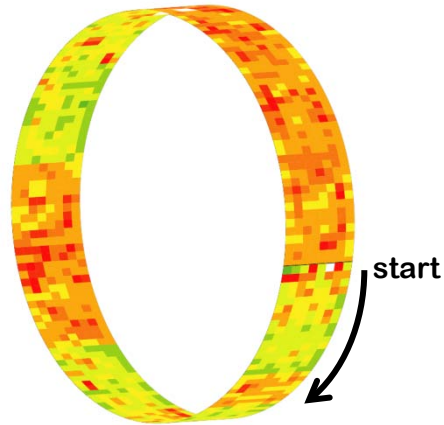
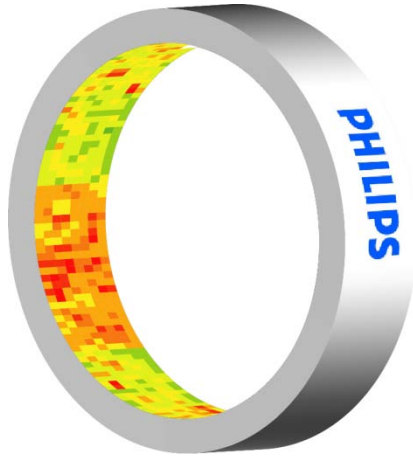
Dimensions of the phantom (in mm)



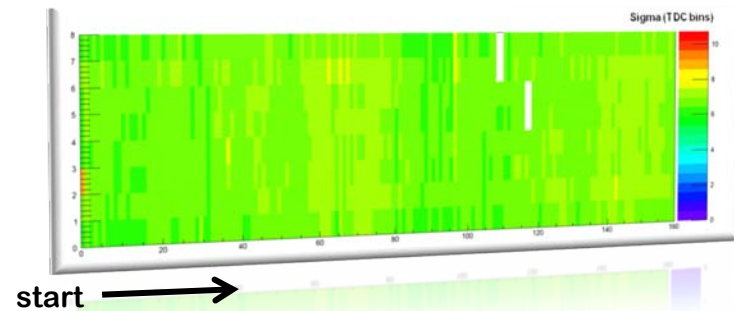
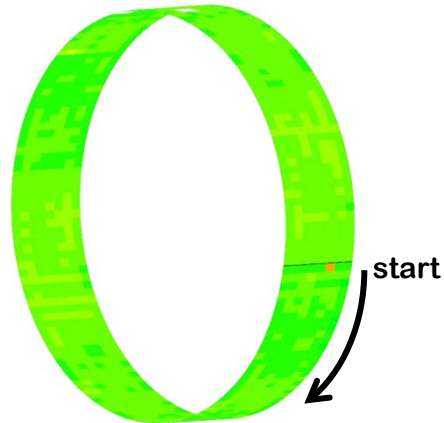
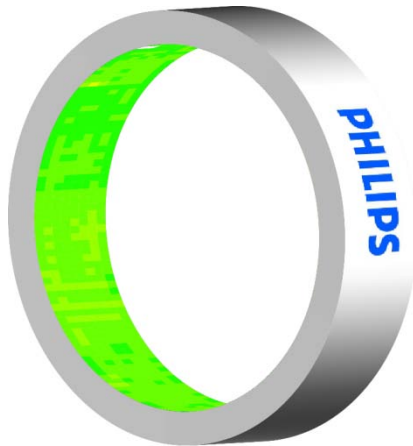
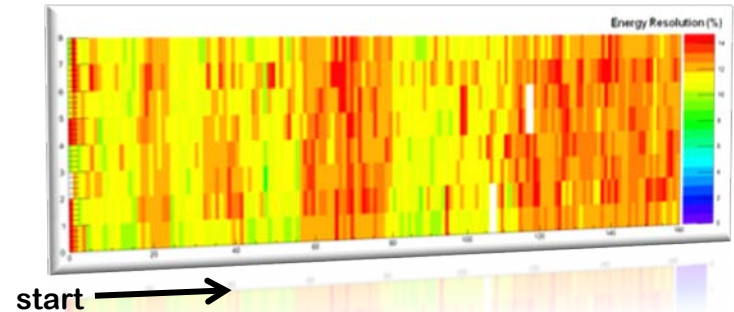
80% contrast recovery for 3mm insert

Interpreting the Plots

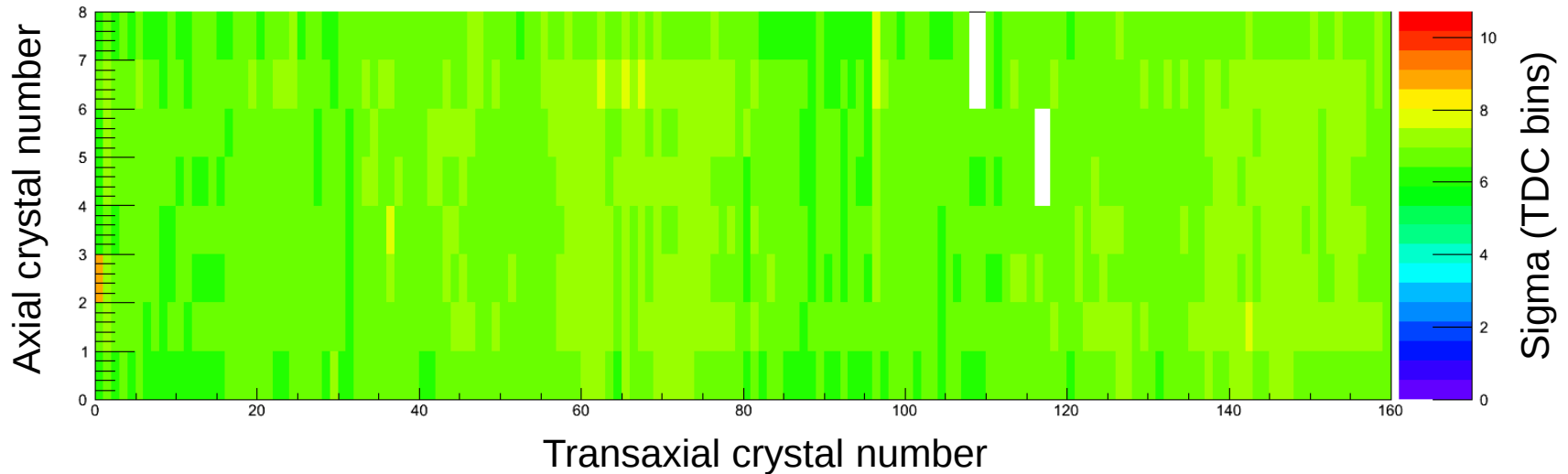
Crystals Occupancy Map



Unfolded Map



Timing Resolution of Prototype Ring



- 3.7 MBq ^{22}Na pointsource
- Coincidence timing resolution (FWHM): 263 ps (± 3.9 cm)

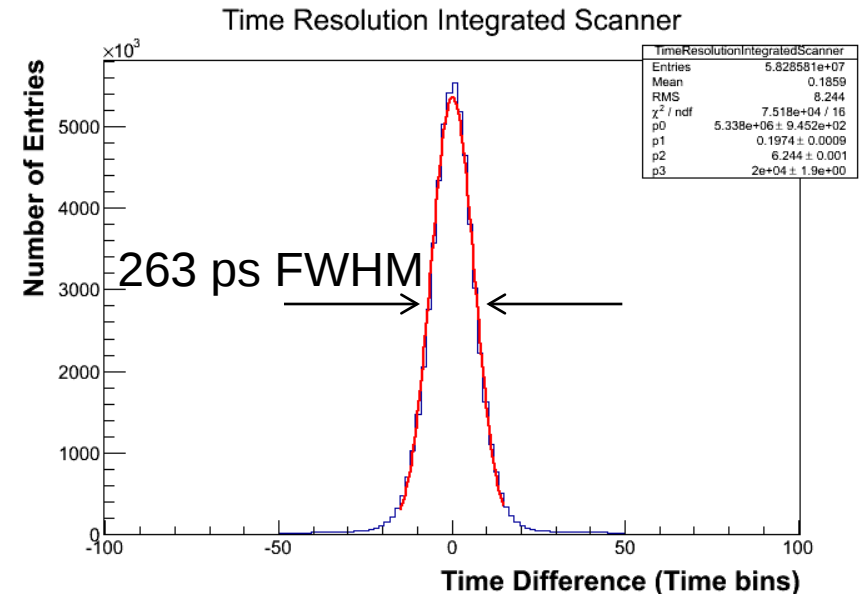
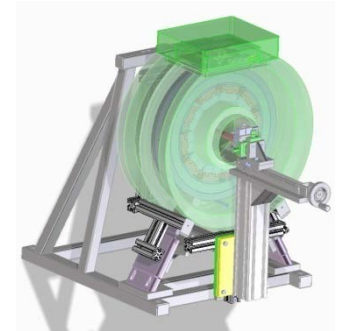


Image Quality Overview



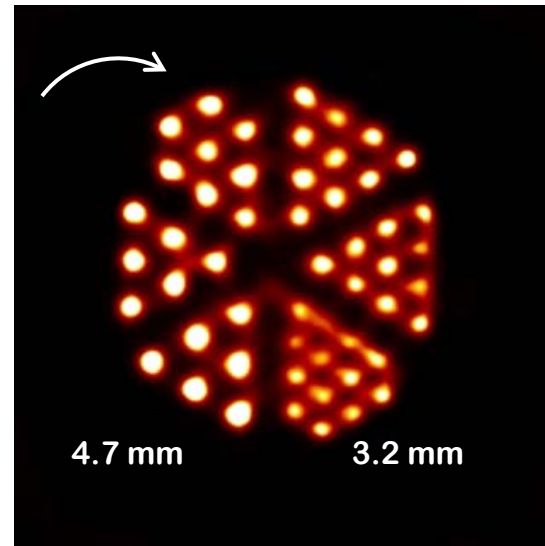
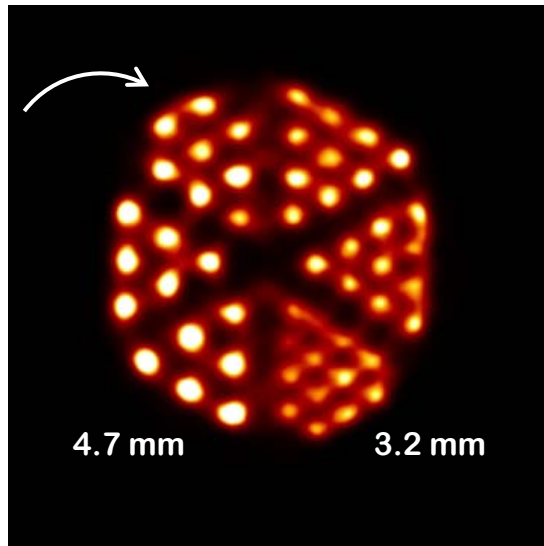
- Hot rod phantom (70 mm diameter)
- 1h data acquisition (10-15 MBq ^{18}F)
- Trigger 2 at 7-9°C (internal tile temperature)
- Energy (RE 13% & clustering) and time (TR 390 ps) calibrations applied
- Energy window of [440;660] keV and time window of 3 ns [-1.5;1.5]



Without TOF

With TOF

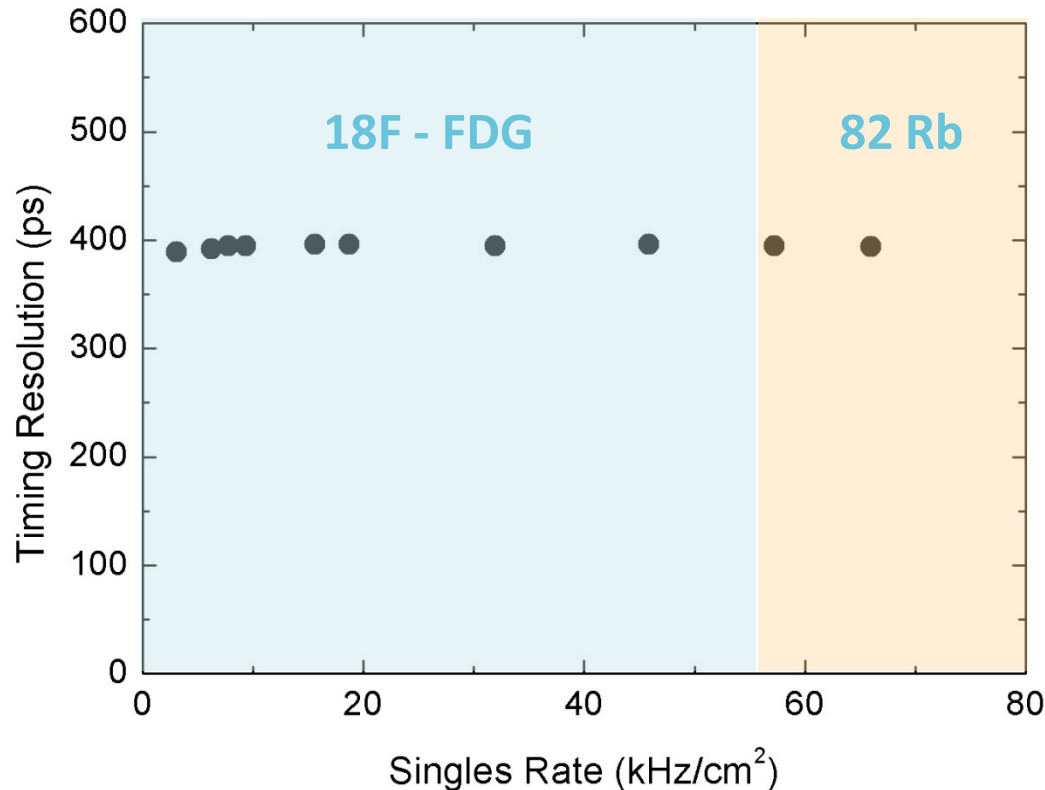
263 ps ($\pm$ 3.9 cm)



PURE/OSEM (0.5 mm voxels), no norm., no decay time, all other corrections applied.

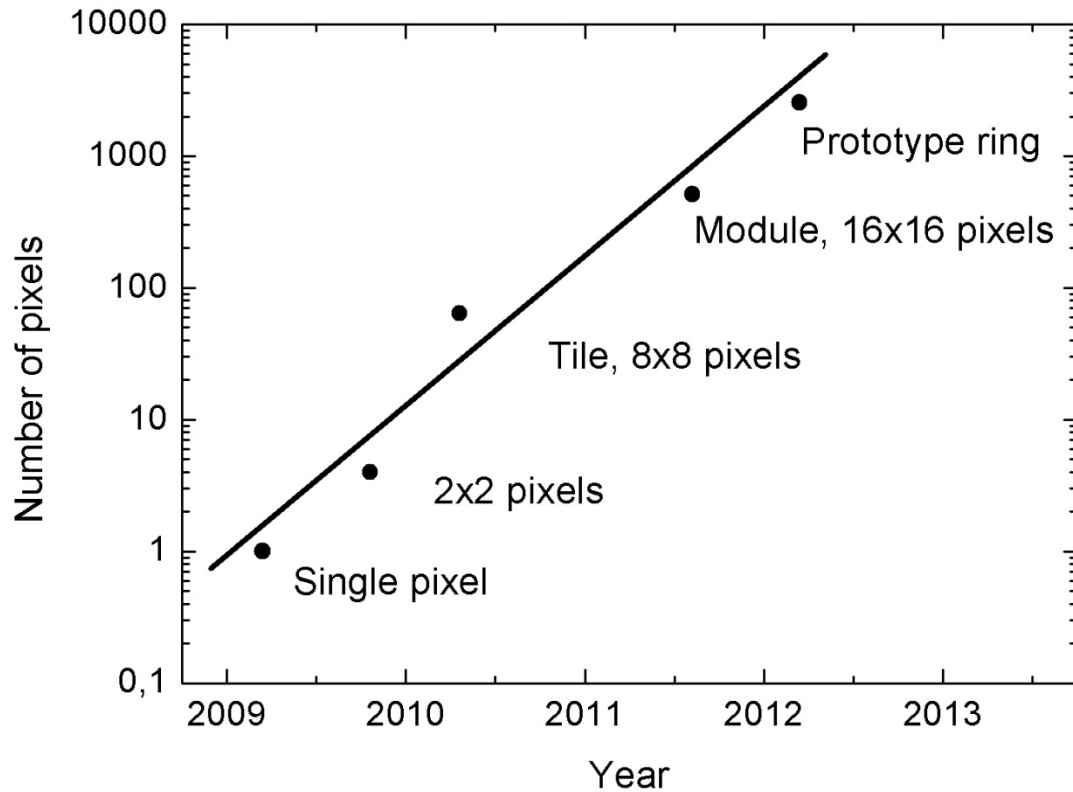
Heraeus Seminar Bad Honnef, May 23rd, 2013

Count Rate Performance of Prototype Ring



- 1:1 coupling between scintillator and detector eliminates pile-up
- No degradation of timing, energy and spatial resolution with activity

Moore's law for PDPC



Coincidence timing
resolution FWHM

Single pixel	250 ps
Ring	263 ps

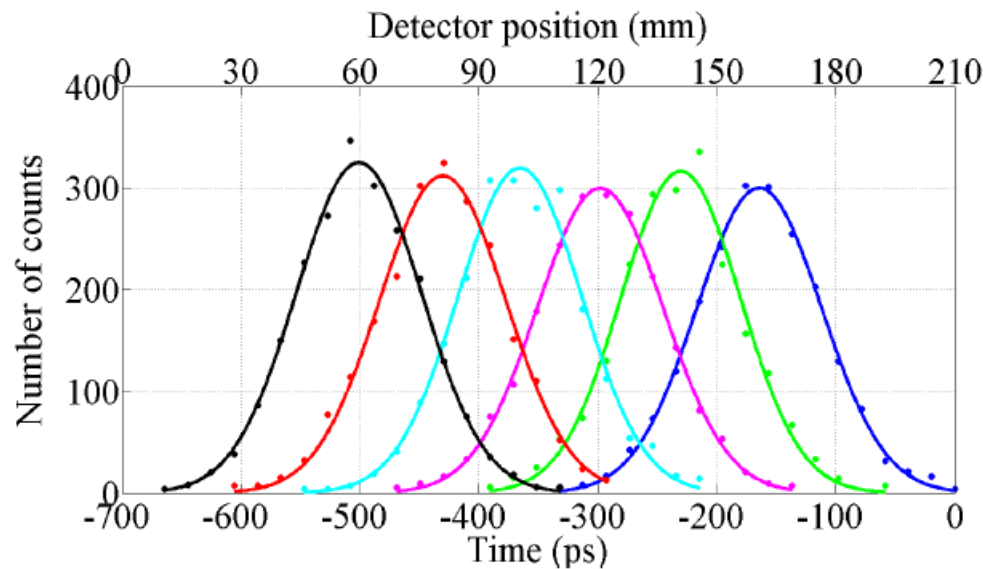
Number of pixels doubled every 3 months, while
maintaining performance

Timing Resolution with Single Short LSO:Ca Crystals

Timing resolution

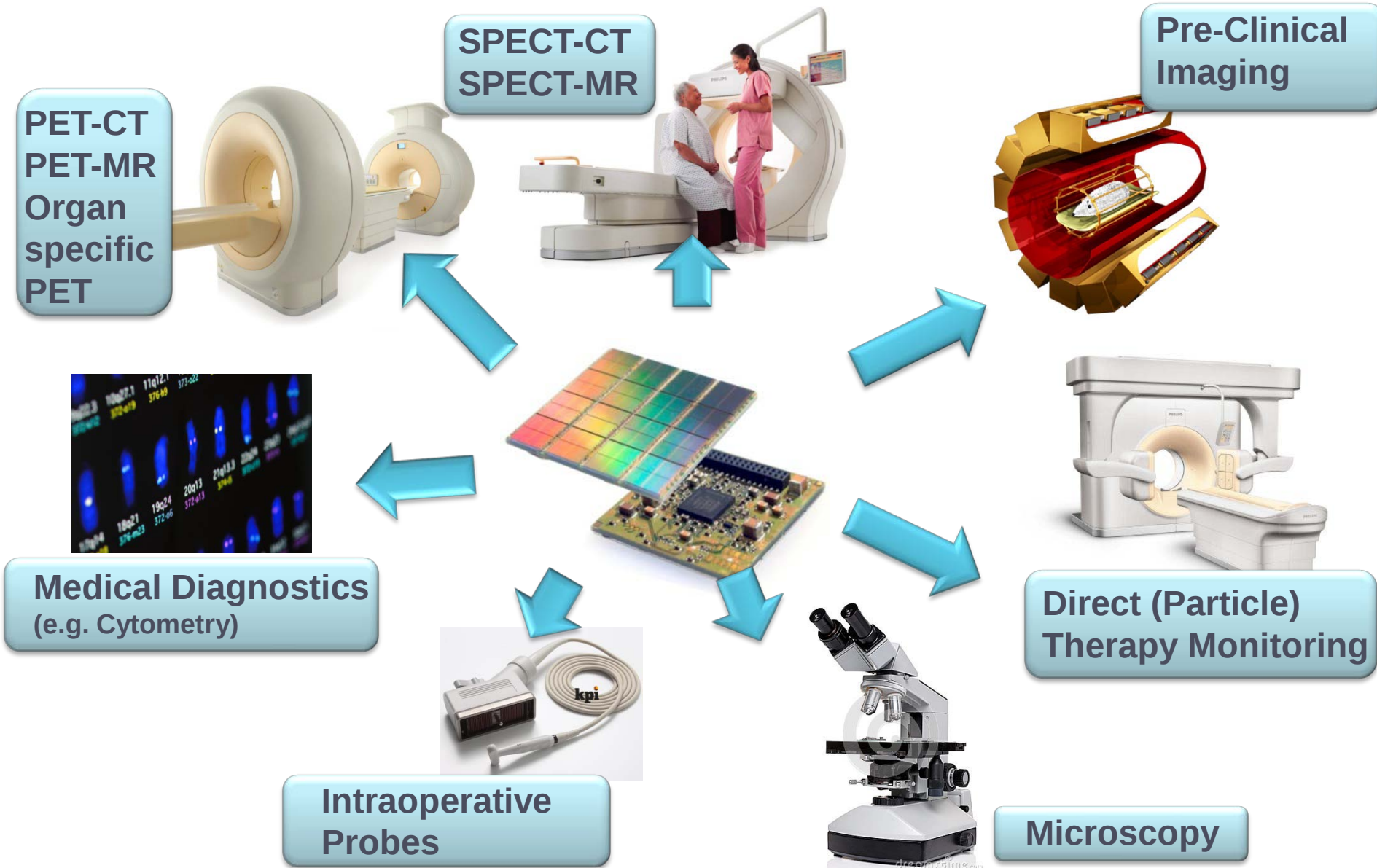
Two coincident detectors:

- DPC-3200-44-22 dSiPM arrays
- $3 \times 3 \times 5 \text{ mm}^3$ LSO:Ce,Ca crystals



Timing spectra at different positions of one of the two detectors. The step size is 20 mm. The average coincidence resolving time (CRT) is **123 ps FWHM**.

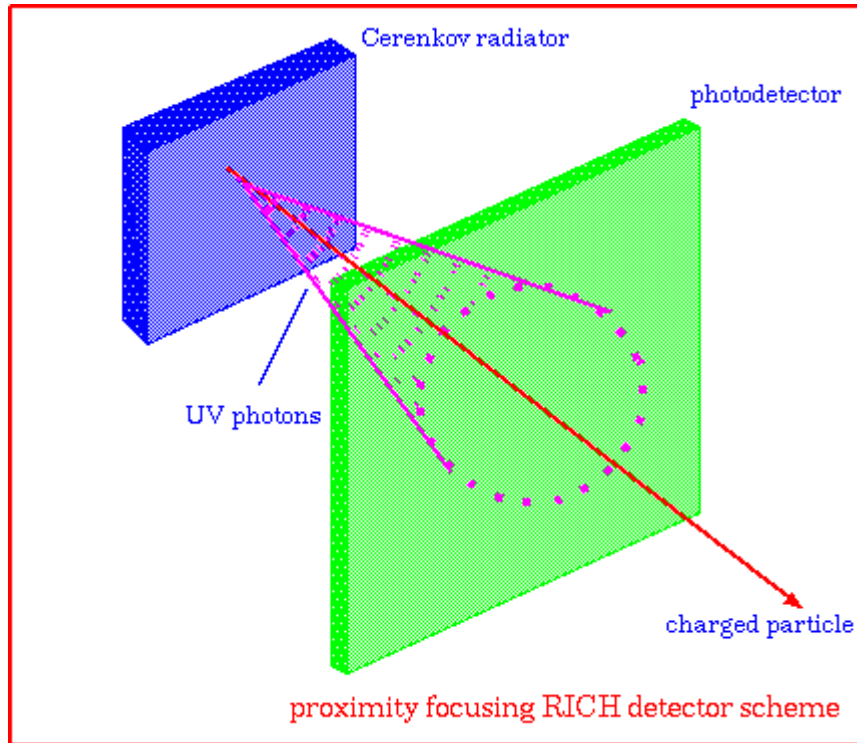
Philips DPC technology: potential in Healthcare



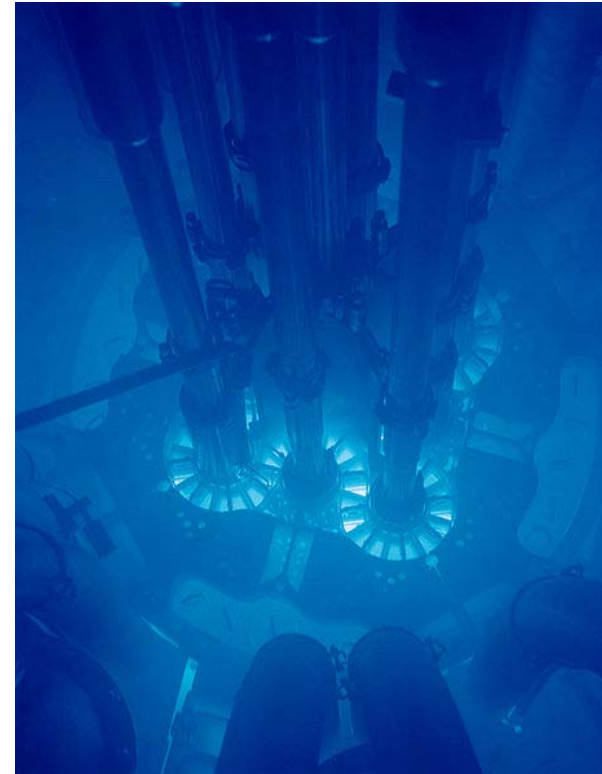
Application Example

Cerenkov Light Detection

Ring Imaging Cerenkov (RICH) Detector

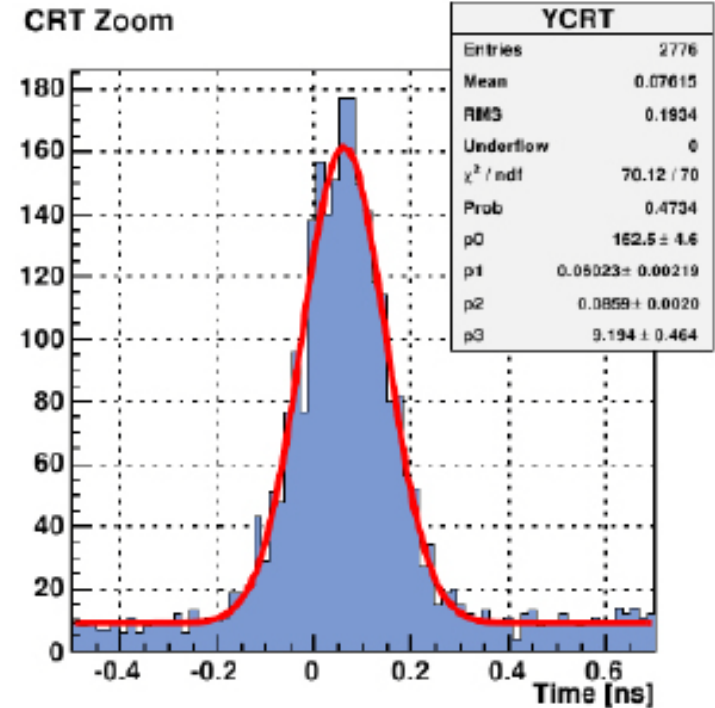
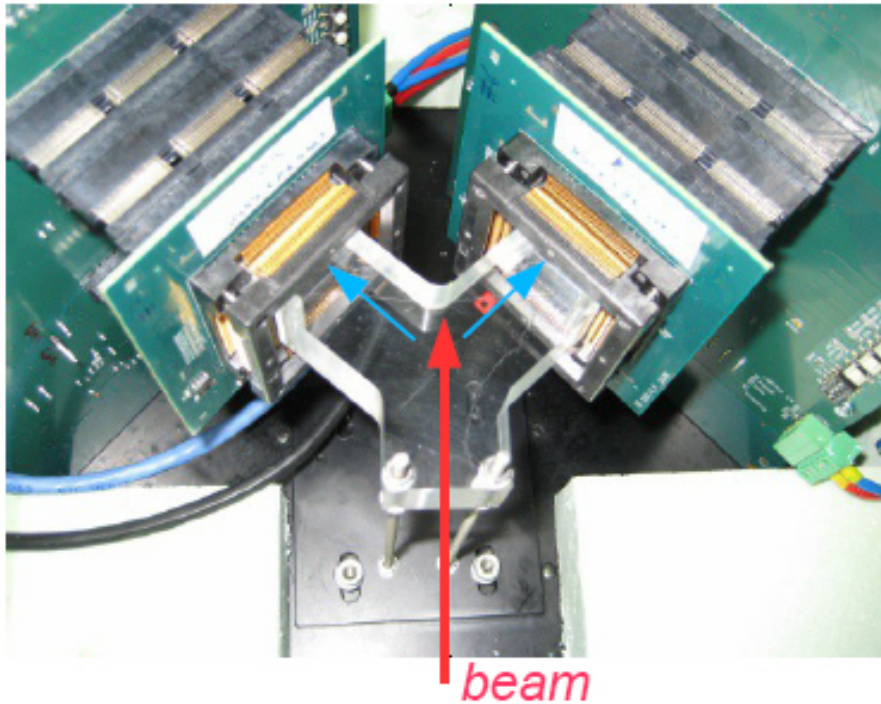


Use Cerenkov radiation for particle identification



Challenge: Detect low number of photons with high timing resolution

DPC: First Use for Cerenkov Detection 2011



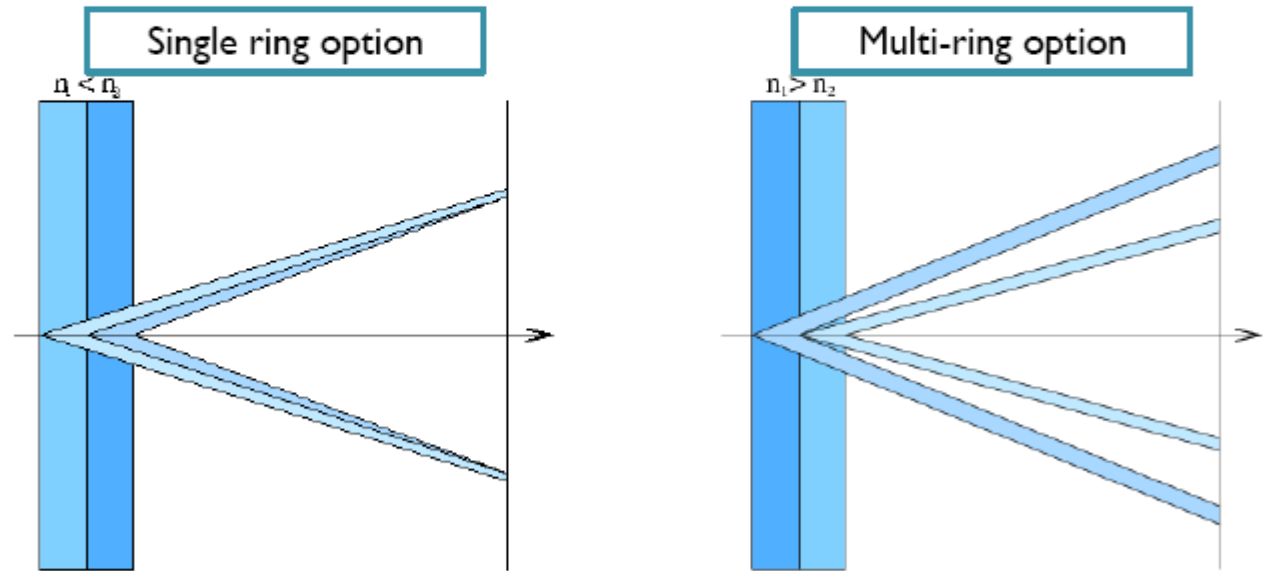
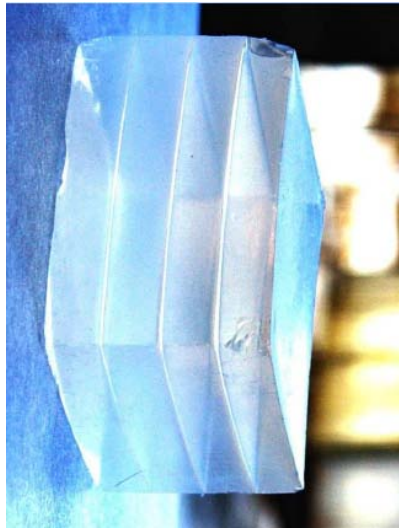
- PMMA radiator coupled via air gap to two dSiPMs (DLD8K) in coincidence
- Box isolated and temperature-controlled with a TEC to 2 – 3°C
- Cooperation between Giessen University (Prof. Düren) and Philips DPC
- First measurements at CERN SPS: $\sigma = 60.7\text{ps}$

DPC in High Energy Physics: FARICH Detector

FARICH concept

Focusing Aerogel RICH – FARICH

Improves proximity focusing design by reducing radiator thickness contribution into the Cherenkov angle resolution



T.Iijima et al., NIM A548 (2005) 383
A.Yu.Barnyakov et al., NIM A553 (2005) 70

13/02/2013 VCI 2013

First test of DPC in High Energy Physics: FARICH Detector @ CERN, June 2012

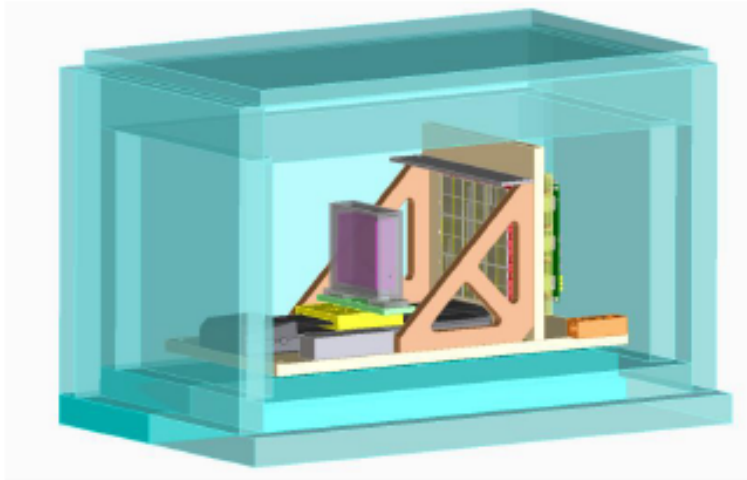
Main objective:

Proof of concept: full Cherenkov ring detection with DPC array

Timeline:

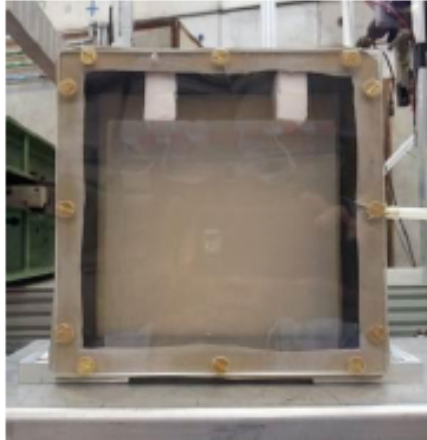
- Started to envisage:
28/02/12
- Requirements for the FARICH prototype test setup fixed: **30/04/12**
- Prototype operational @ Aachen Labs: **03/06/12**
- Installed @ CERN: **12/06/12**
- Subsequent beam runs for 12 days until **25/06/12** with smooth setup operation

Fast prototyping!



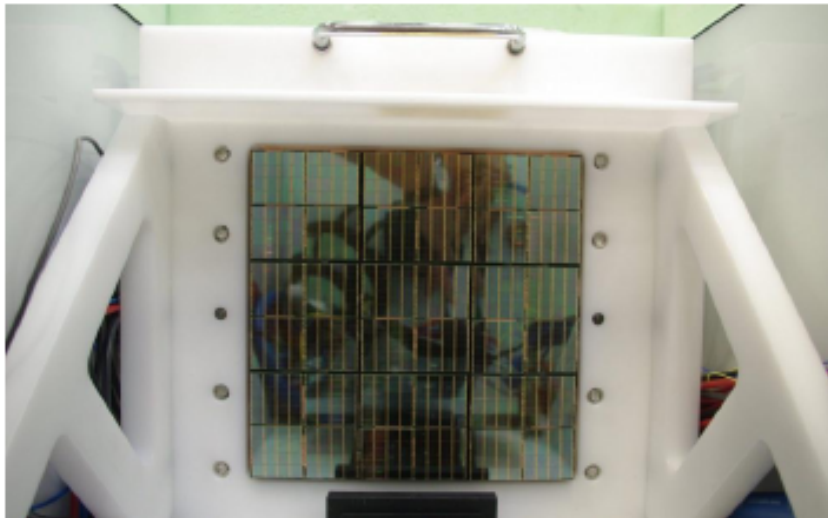
13/02/2013 VCI 2013

FARICH prototype with DPC...



4-layer aerogel

- $n_{\max} = 1.046$
- Thickness 37.5 mm
- Calculated focal distance 200 mm
- Hermetic container with plexiglass window to avoid moisture condensation on aerogel



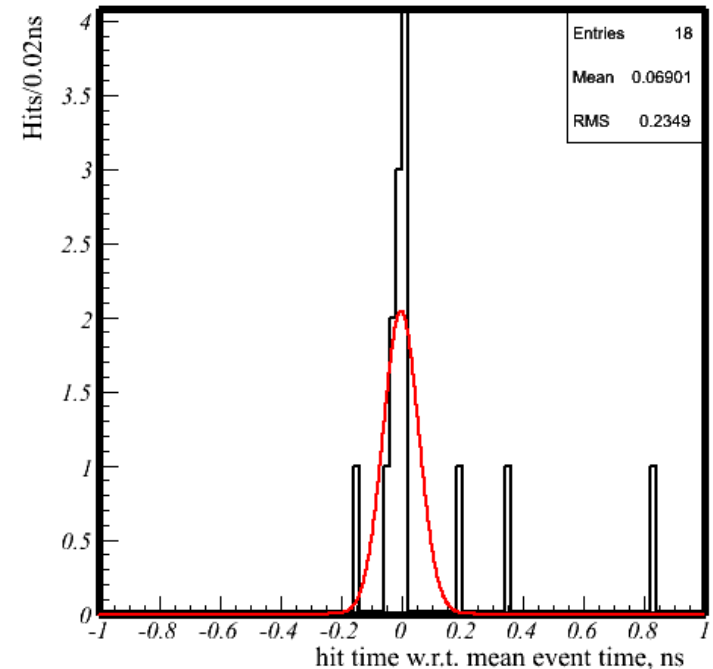
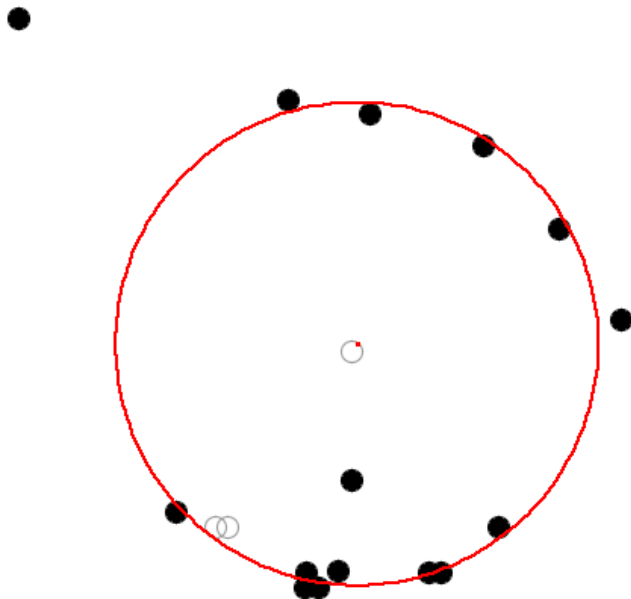
Square matrix **20x20 cm²**

- Sensors: DPC3200-22-44
- 3x3 modules = 6x6 tiles = 24x24 dies = 48x48 pixels in total
- 576 time channels
- 2304 amplitude (position) channels
- 4 levels of FPGA readout: tiles, modules, bus boards, test board

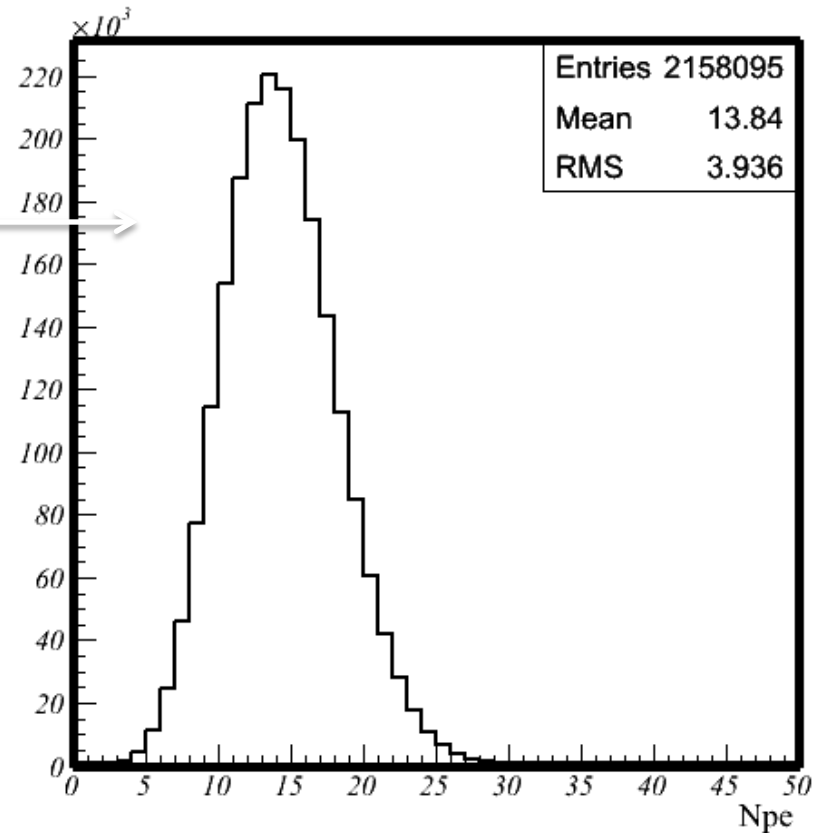
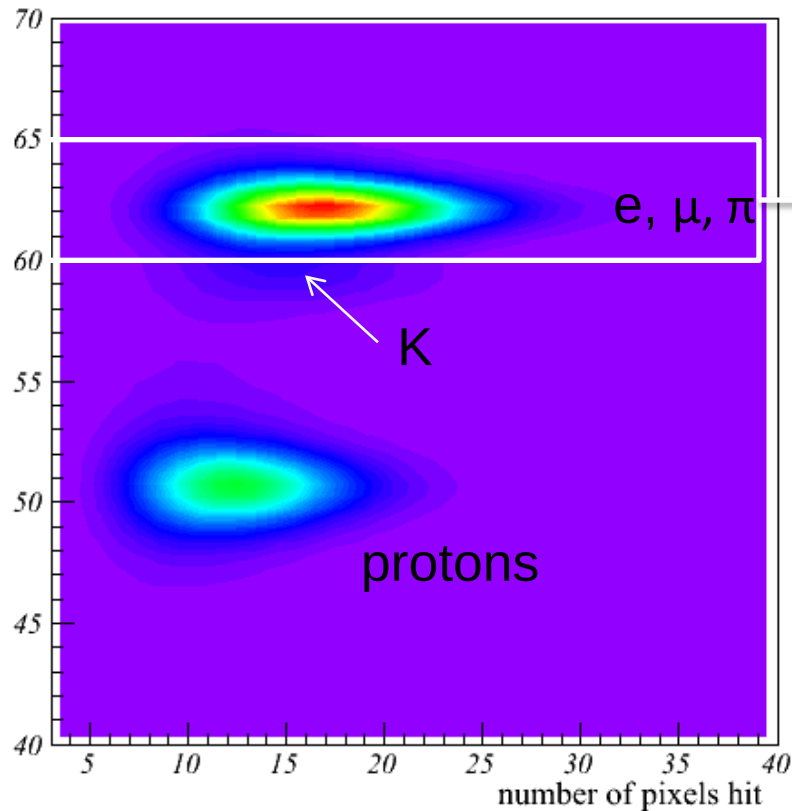
Event-by-event ring fit

Hit selection and ring fit:

- Reject central hits
- Select hits in 4 ns time window
- More than 3 selected hits per event
- 4 parameters fitted: X_{center} , Y_{center} , R , t_0



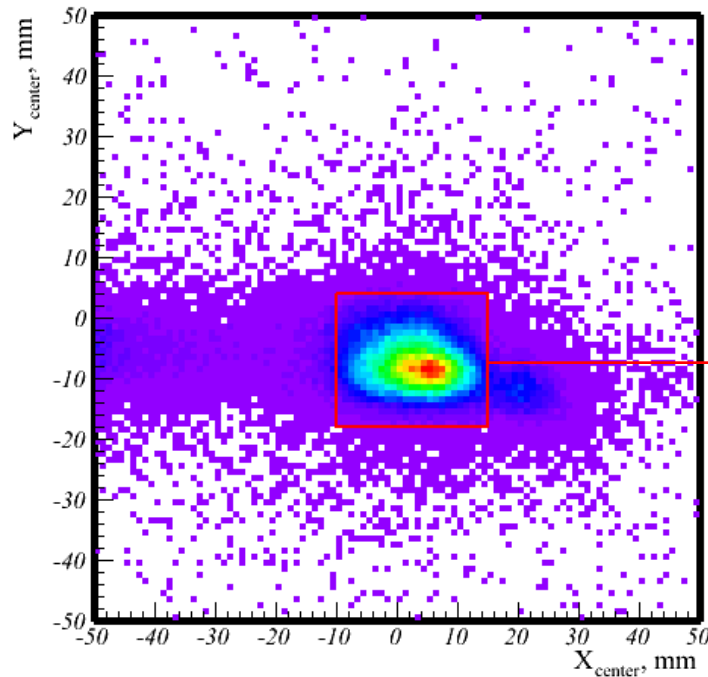
Number of photoelectrons



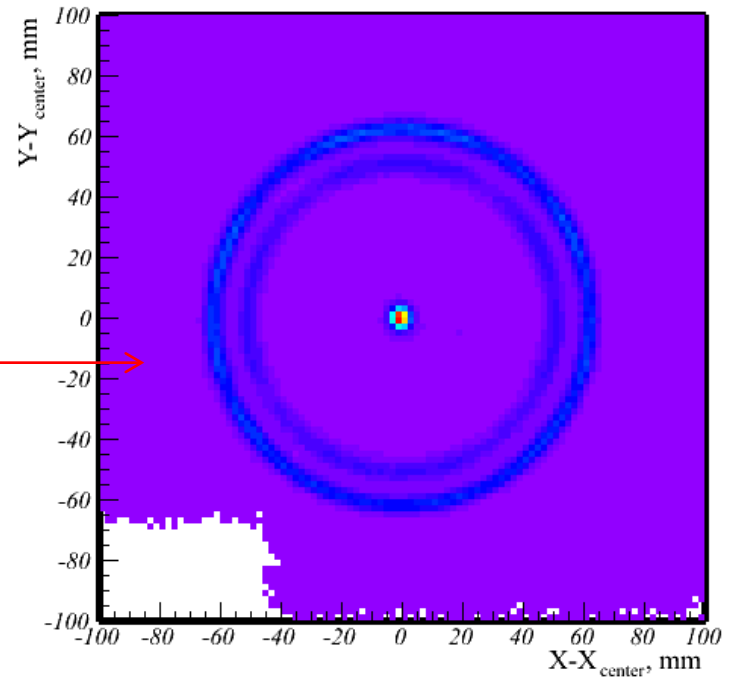
Ring center adjusted distributions

$P=6 \text{ GeV/c}$, $L=200\text{mm}$

Ring center position
in detector plane



Hit positions



Ring radius distribution fit

Fit function

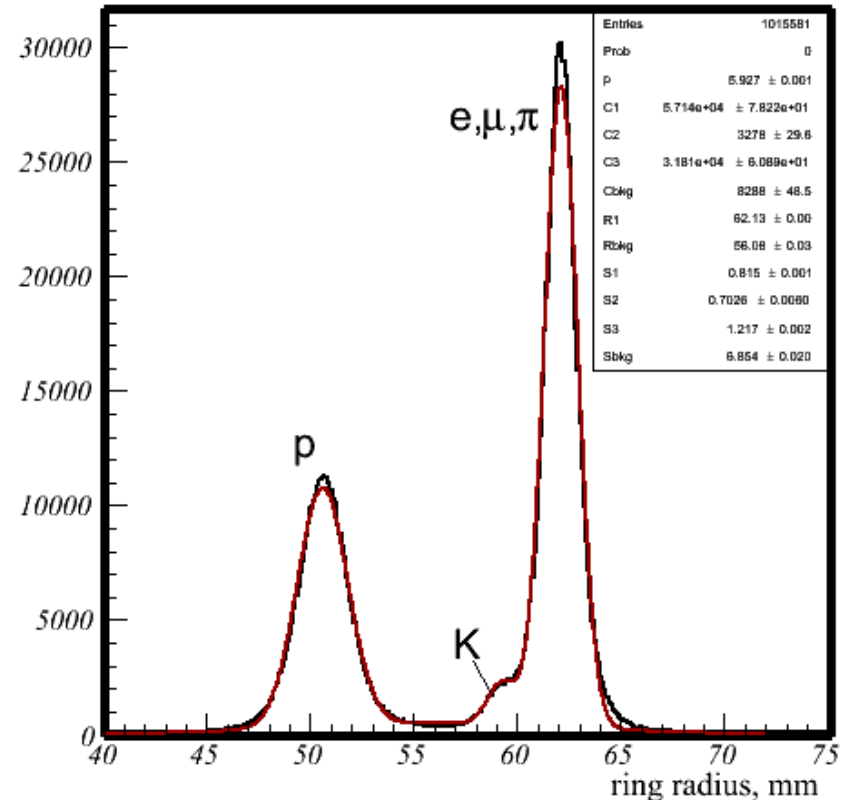
sum of **three gaussians** for each particle type with distinct radius plus **gaussian background** (to account for non-monochromatic particles in the beam)

Free parameters:

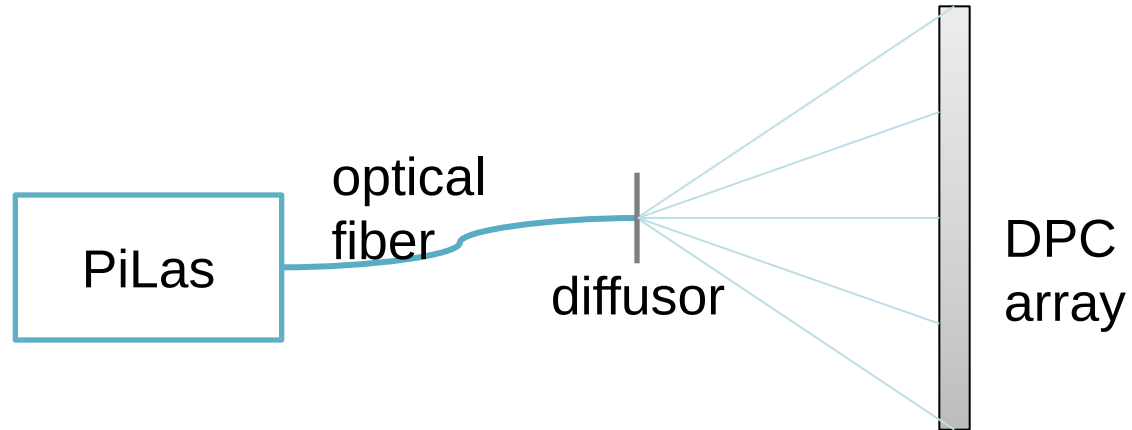
- Particle momentum
- Ring radius of rightmost gaussian (other radii derived from Cherenkov law)
- Constants and sigmas of all gaussians

Fixed parameter:

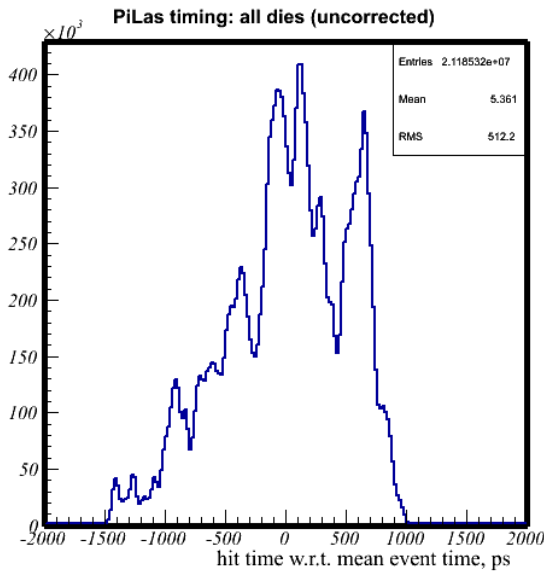
- Effective refractive index
 $n_{\text{eff}}=1.038$



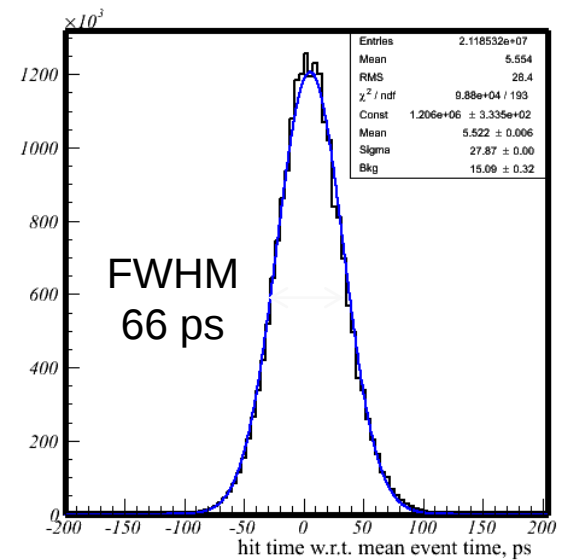
Die-to-die clock skew correction



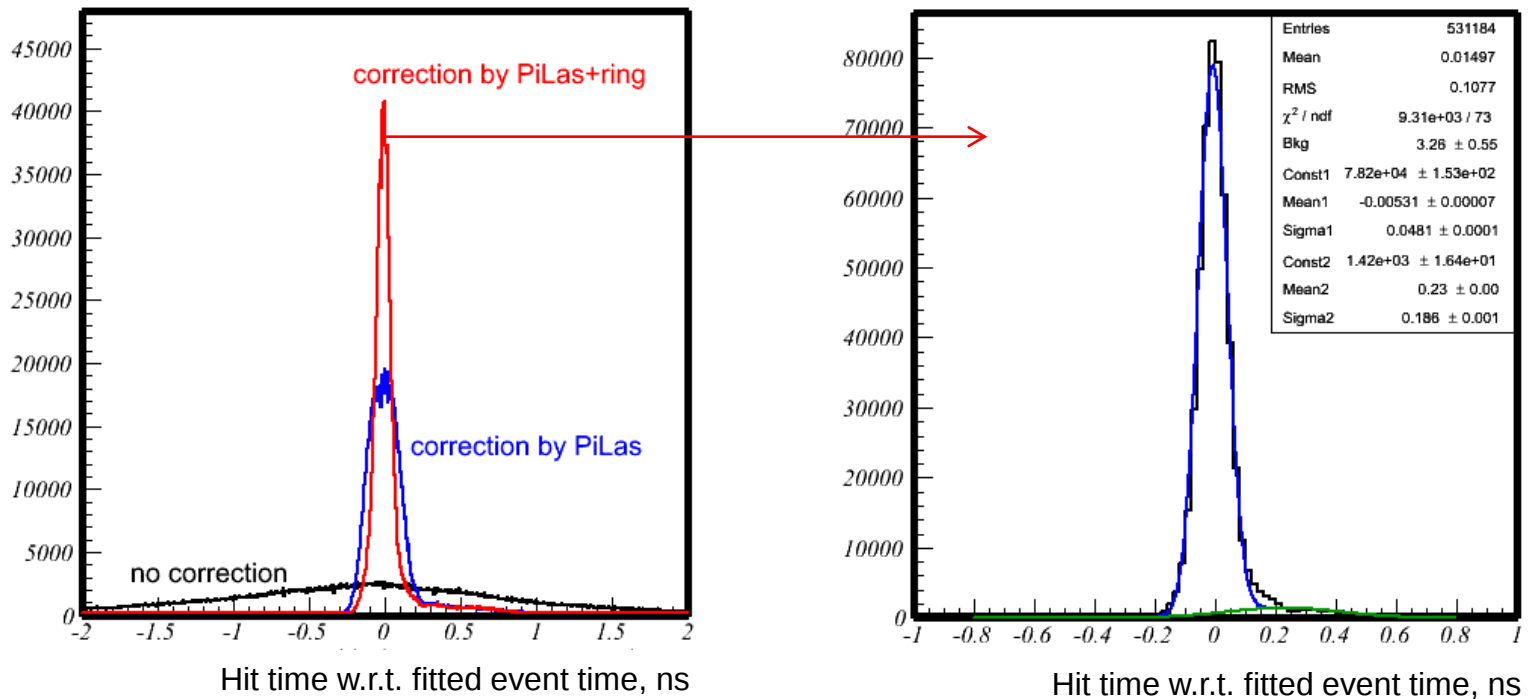
All dies hit times w.r.t. mean event time



Clock skew
correction
between dies



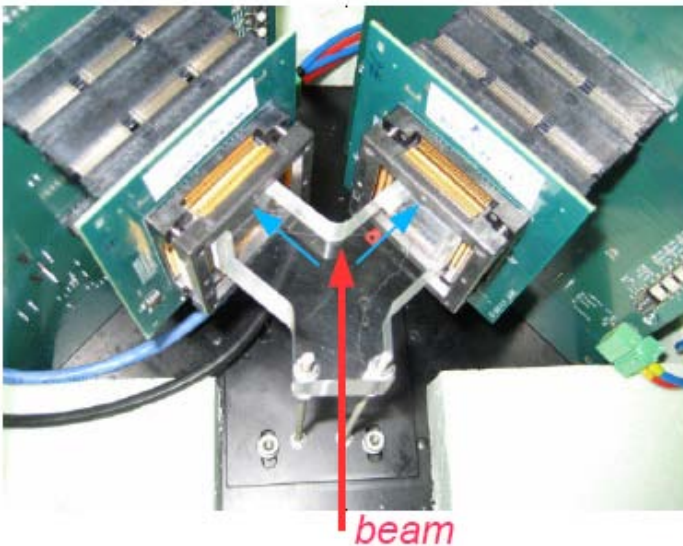
Timing resolution for Cherenkov photons



$$\sigma = 48\text{ps}$$

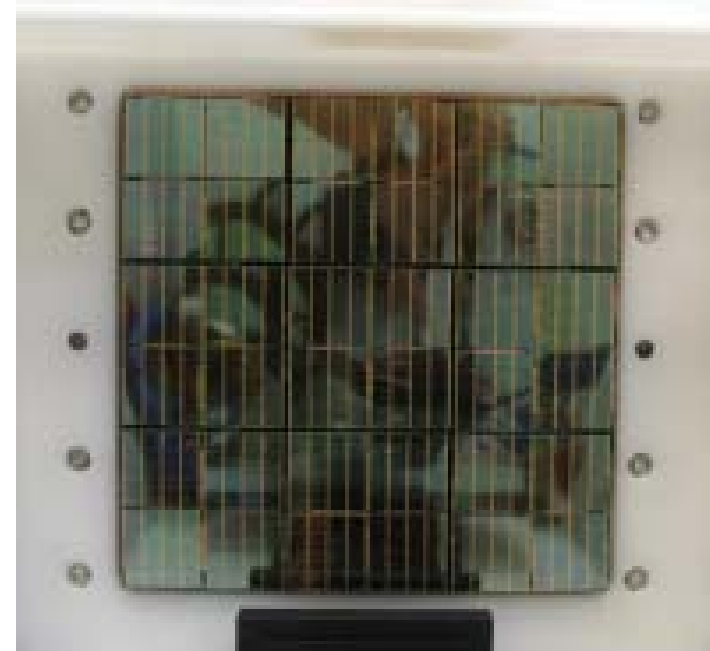
Comparison of timing resolution

Single pixel, 4 x 4 mm²



$$\sigma = 61 \text{ ps}$$

System, 2304 pixels, 200 x 200mm²



$$\sigma = 48 \text{ ps}$$

Scalability of timing performance shown

There are large detectors (not only) @ CERN



PDPC Technology Evaluation Kit (TEK)



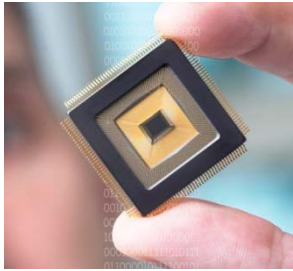
25 kits installed so far

Application Example

Outlook

DPC technology concept beyond PET

- The first target application for dSiPM technology is ToF-PET. (Time-of-Flight Positron Emission Tomography).
- The first DPC sensor family (e.g. DPC 6400-22 / DPC3200-22) may be usable in other applications for scintillation light detection.



Die



Tile



Module



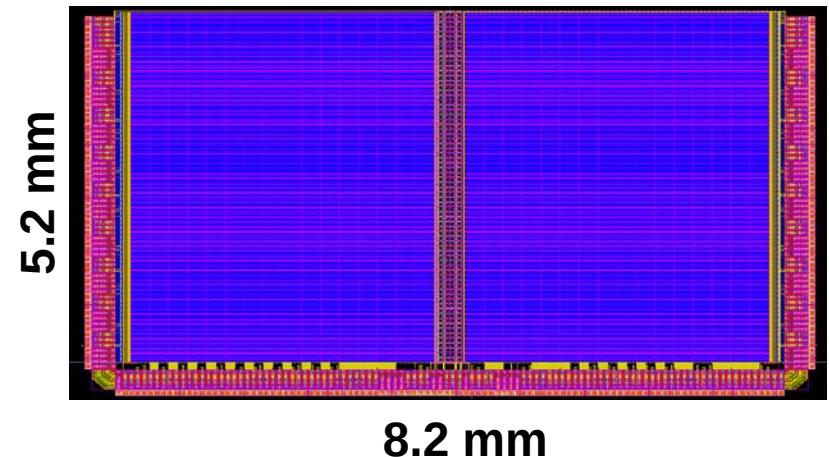
PET Ring

How can DPC technology be adapted to other applications?

➡ **Pathfinder : design new sensors and modular packaging for new applications using DPC technology**

Functional test of a line sensor with SPAD technology suitable for LIDAR (**Light Detection and Ranging**) or 3D scan imaging applications and FLIM (**Fluorescence Lifetime Imaging**).

- 72-line sensor is implemented
- 1 line = Cell-Diodes + TDCs
- Each 8-lines has its clock and data channels
- stitch-able design for e.g. a 144 line sensor

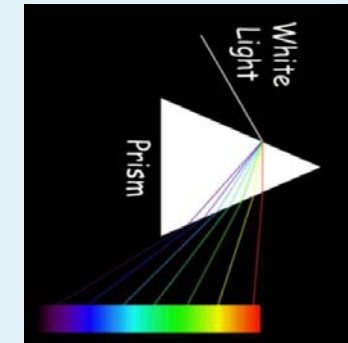
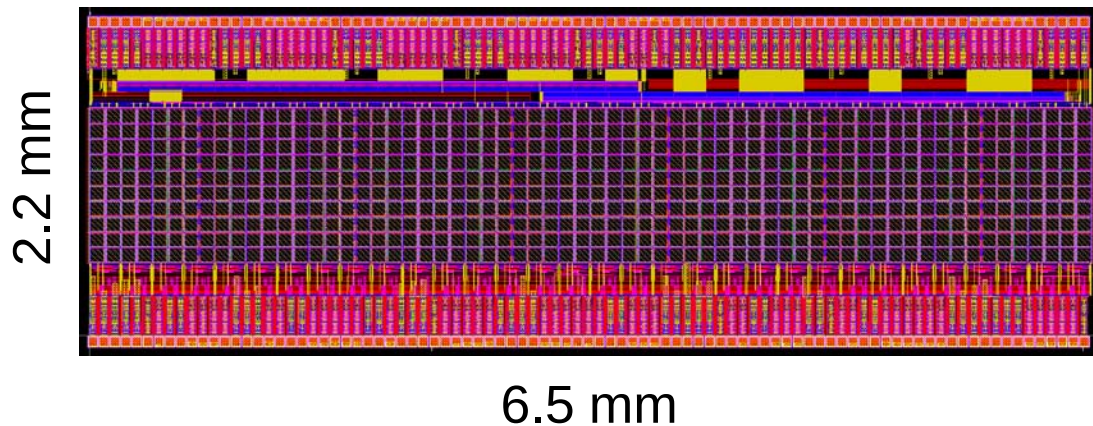


DPC technology concept extension: spectroscopy

Objective:

- Functional test of the line sensor with SPADs for **fluorescence detection** and **spectroscopic applications**
- Industrial and Biological **Spectroscopy** applications
- Confocal **Raman Spectroscopy**
- Fluorescent lifetime imaging (**FLIM**)
(one programmable TDC is implemented to perform the timing measurement of the first photon hit)

64 x 10 Geiger mode diodes



<u>0</u>	<u>0</u>	<u>1</u>	<u>1</u>	<u>0</u>	<u>0</u>	<u>0</u>
<u>0</u>	<u>0</u>	<u>1</u>	<u>1</u>	<u>1</u>	<u>0</u>	<u>0</u>
<u>0</u>	<u>1</u>	<u>0</u>	<u>1</u>	<u>0</u>	<u>0</u>	<u>0</u>
<u>0</u>	<u>0</u>	<u>1</u>	<u>1</u>	<u>0</u>	<u>0</u>	<u>0</u>

SPAD array Programming logic

Programmable TDC

Simplified Architecture
(with example excitation)

Summary/Outlook

- Demonstrated **scalability** of Philips DPC technology by maintaining intrinsic performance:
 - *PET test ring*
 - *FARICH detector prototype*

OUTLOOK/Next:

- **Expansion of Scale** of technology:
 - *detectors with larger number of pixels*
 - *additional building blocks of scalable architecture*
- **Improved performance** of DPCs (2nd generation):
 - *higher PDE (>50%)*
 - *less dead time (factor 10)*
 - *better intrinsic timing resolution (factor 2)*
 - *subpixel (2x2 mm²) readout*
- **New designs** for new applications
 - *line- and image sensors*
 - *LIDAR, FLIM, Spectroscopy*

Thank you very much for your attention!

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PET

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