A beam hodoscope for ion therapy monitoring by means of secondary radiations

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#### Introduction

hadrontherapy = tumor treatment with protons or carbon ions

#### conventional radiotherapy vs hadrontherapy



[D. Schardt Rev. Med. Phys. 2010]

- Bragg peak
- higher RBE relative biological effectiveness



## The Heidelberg Ion Therapy center (HIT)



[Th. Haberer Cern Accelerator School 2012]





#### Hadrontherapy worldwide





- ► 55 centers in operation
- 34 centers under construction
- 16 centers in planning phase
- ► strong growth in the number of centers [http://www.ptcog.ch/]

## Hadrontherapy: sensitivity to range uncertainties



[Knopf et al. Phys. Med. Biol. 2013]

- ► safety margins (≈ 3 % + 1.2 mm) [H. Paganetti PMB 2012]
  - ⇒ full potential not yet exploited
- ► ⇒ online monitoring highly desired

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#### Nuclear reactions phases and products



- projectile-like and target-like fragments
  e.g. β<sup>+</sup> emitters: <sup>11</sup>C, <sup>15</sup>O, ...
  ⇒ PET monitoring (offline)
- ► prompt γ-rays, neutrons, light charged particles ⇒ real-time monitoring
- high probability (for ranges ~10 cm) ~10% for protons, ~40% for carbons

## **PET** monitoring





- detection of gammas (positron annihilation)
- activity distributions
- p: target fragments
- <sup>12</sup>C: from projectiles
- biological washout

[Enghardt et al. NIM A 2004]



#### Prompt secondary radiation for ion range monitoring emission yields (Geant4 9.4) typical treatments (PBS)



	number of ions	
	(distal slice)	
	proton	carbon
energy slice	$\sim 10^{10}$	$\sim 10^{8}$
single spot	$\sim 10^8$	$\sim 10^{6}$

[Krämer PMB 2000], [Grevillot PMB 2011], [Smeets PMB 2012]

- correlation between ion range and nuclear reaction depth profile
- radiation for real-time monitoring of the ion range:
  - prompt γ-rays (energy up to ~10 MeV
  - light charged particles (mainly from projectile fragmentation)

#### Hadrontherapy: Context

#### Beam parameters

- proton therapy: cyclotron (e.g IBA C230)
  - bunch length: 2 ns
  - time between bunches: 10 ns
  - 200 protons per bunch
- carbon ion therapy: synchrotron (HIT/CNAO)
  - bunch length: 20-40 ns
  - time between bunches: 200 ns
  - 10 ions per bunch

#### Specifications for beam monitoring

- count rate: 100 MHz
- time resolutions: 1 ns
- spatial resolution: 1 mm
- irradiated matrix: 15×15 cm<sup>2</sup>

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## Hadrontherapy: real-time monitoring



## Common device: beam tagging hodoscope

- ▶ goals:
  - -position resolution 1 mm -time resolution 1 ns -count rate 10<sup>8</sup> 1/s
- array of scintillating fibers (1×1 mm<sup>2</sup> BCF 10/12)



- prototypes: 2×32 and 2×128 fibers
- readout: optical fibers FORETEC
- coupling to multianode PM H-8500



## Hodoscope: performance tests

- ► GANIL: 75 MeV/u <sup>13</sup>C, IPN Orsay: 25 MeV protons
- ► time reference: cyclotron HF ⇒ time resolution 1 ns FWHM



- ► H-8500 ⇔ MCP-PMT
- max. rate > 10 MHz, for H-8500 at 800 V
- ► MCP-PMT at 2200 V ⇒ less performant



#### Hodoscope: distribution of signals

- distribute signals from neighboring fibres to different PMs
  increase of maximum count rate
- read fibres from both sides:
  - $\Rightarrow$  increase of efficiency
  - $\Rightarrow$  timing independent on hit position





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$$t_A = \frac{x}{c}, \ t_B = \frac{L-x}{c}$$
$$t = \frac{1}{2} (t_A + t_B) = \frac{1}{2} \frac{L}{c}$$

## Hodoscope: Test bench for multianode PMs

- 8 PMs H-8500 to characterize
- 64 channels each
- LED on translation table
- reference PM to compensate for variations
- automatic measures via LabView
- variation in gain for different pixels factor 2-3



## Hodoscope: front end electronics

- goals: rate 10<sup>8</sup> 1/s, time information, analog output (monitoring of fiber aging)
- first version of ASIC:
  - current comparator
  - CSA
  - S. Deng et al. NIM A 695 (2012)
- second version of ASIC:
  - inclusion of time stamper
  - 160 MHz clock + DLL
  - 32 to 5 Gray encoder

 ASIC + DAQ card tested final version in production





# Fast DAQ system: µ-TCA acquisition diagram



[C. Abellan ICTR-PHE 2014]

#### $\mu$ -TCA crate



#### AMC board (CPPM)



(a)

- front-end electronics: IPNL Lyon, LPC Clermont
- AMC board: CPPM Marseille

Alternative approach: Diamond detectors

#### MONIDIAM project (LPSC Grenoble)

- fast response, high count rate capability
- radiation hardness
- production: PECVD (Plasma Enhanced Chemical Vapor Deposition)
- maximum size:
  - $50 \times 50 \text{ mm}^2$  polycrystalline,  $7 \times 7 \text{ mm}^2$  monocrystalline
- tests: <sup>241</sup>Am source (alpha 5.4 MeV) 95 MeV/u <sup>12</sup>C at GANIL
- perspectives: ASIC development, thinning to 200-300 μm



#### prompt- $\gamma$ detection with collimated detectors



#### prompt- $\gamma$ detection with collimated detectors



## prompt- $\gamma$ detection with collimated detectors



target

- on a moving table
- ▶ PMMA, H<sub>2</sub>O, ...

#### collimator

material: tungsten, Pb

scintillation detector

LaBr<sub>3</sub>, LYSO, BGO, ...

Time-of-Flight (TOF) measurements

- reduction of neutron background
- time reference:
  - monitor detector intercepting the beam (synchrotron)
  - accelerator HF (cyclotron)



## prompt- $\gamma$ profiles: heterogeneous targets 95 MeV/u <sup>12</sup>C (GANIL)



▶ influence of heterogeneities close to Bragg peak
 ⇒ change in ion range

[M. Pinto et al. Med. Phys. 2015]

## prompt- $\gamma$ profiles: multislit collimator



#### <sup>13</sup>C 75 MeV/u (GANIL)



[J.K. et al. JINST 2015]

- carbon beams at GANIL and GSI
- ▶ prompt-γ profiles
- ► inter-detector scattering ⇒ contribution < 10 %</p>

## Collimated cameras: multislit (IPNL)





- collimator optimized for falloff retrieval precision
  ⇒ expected σ ~ 1 mm for 10<sup>8</sup> protons (= 1 spot)
  [M. Pinto et al. PMB 2014]
- 20 cm height (2 layers)
- BGO detectors



## Compton camera (TOF): principle



- ► idea: replace passive by *electronic* collimation ⇒ potential increased efficiency
- 3 D information available
- here: line / cone intersection
- components: hodoscope, scatterer, absorber

#### Compton camera: components

beam tagging hodoscope



scatter detectors













- streaked BGO
  64 pseudo pixel
- total 96 crystals
- LPC Clermont

IPNL Lyon, LPC Clermont, CPPM Marseille

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[J.K. et al. NIM A 2015]

#### Components: scatter detector

- double sided silicon strip detectors
- size: 90×90×2 mm<sup>3</sup>
- 7 planes in total
- 2×64 strips (p- and n-side)
- Front-end electronics ASICs (8 ch.), low noise, 1×10<sup>5</sup> cts/s slow (1 µs) and fast (15 ns) shaping
- cooling system





#### Scatter detector: leakage currents





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## Scatter detector: front end electronics specifications

- dynamic: 3.10<sup>3</sup> 3.10<sup>6</sup> e<sup>-</sup>
- count rate: 10<sup>5</sup> 1/s
- low noise: 120 e<sup>-</sup> RMS (1 keV FWHM)
- shaping: 15 ns and 1 μs
- selection: electron / holes

#### scheme of ASIC for SSD:





⇒ switched system

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#### Components: absorber





- streaked BGO crystals 35×38×30 mm<sup>3</sup> read by 4 PMs
- ► 8×8 (pseudo)-pixel, 96 crystals in total
- energy resolution 17% at 511 keV, time resolution 2 ns
- detector assembly and readout electronics: LPC Clermont
- position reconstruction via centroid





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#### proton IVI Simulations (head like phantom) [P. Henriquet et al. PMB 2012]



- various <sup>12</sup>C energies
- fit of error function
- Inflection Point Position
- correlation with energy
- ion range monitoring
- millimetric precision for homogeneous target, single-spot basis (PBS)



#### proton IVI measurements: homogeneous targets



- CMOS detectors: MIMOSA 26 IPHC Strasbourg
   massurement at HI
  - measurement at HIT

#### [V. Reithinger et al. PTCOG 2013]



#### proton IVI measurements: heterogeneous targets



- measurements at HIT
- target: PMMA cylinder with inserts "bone" and "air"
- normalization to integrals

■ "air" inserts at 3 positions ⇒ dip at insert position



[R. Rescigno ICTR-PHE 2014]

## Summary

beam tagging hodoscope

- scintillating fibers
- diamond detectors
- ion therapy monitoring
  - prompt- $\gamma$  detection: collimated- and Compton camera
  - charged particles: proton IVI

#### Outlook



- towards clinical application
- realistic phantoms
- ► improvement of simulations ⇒ prediction of signals

#### thank you very much for your attention

#### collaborators / institutions

- IPNL Lyon
- CREATIS Lyon
- IPN Orsay
- LPC Clermont
- CPPM Marseille
- IPHC Strasbourg

- CAL Nice
- GANIL Caen
- HIT Heidelberg
- GSI Darmstadt

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- WPE Essen
- IBA

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## backup: proton radiography (proton CT)



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#### backup: Time-of-Flight PET



 $\Delta x = c \Delta t/2$ 100ps resolution  $\Leftrightarrow$  1.5 cm

► use of TOF information ⇒ increased SNR

## backup: In Beam TOF-PET

- small activity produced, in comparison to diagnosis
- short half lifes: <sup>11</sup>C (20 min.), <sup>15</sup>O (2 min.),...
- preferred solution: in beam TOF-PET with sub-ns time resolution
- study of configurations and detection methods
  - scintillator-based TOF-PET
  - RPC-based TOF-PET (MRPC)
- Coincidence Resolving Time CRT in the order of 200 ps



[Amaldi et al. NIM A 2015]



## backup: Collimated cameras: knife-edge (IBA)





- principle: slit-hole camera
  [Bom PMB 2012]
- prototype optimization: falloff retrieval precision
   1 mm for a distal spot [Smeets PMB 2012]
- tests with prototype and IBA C230 cyclotron
   [Perali PMB 2014]
- investigations with anthropomorphic phantoms in progress